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1 **Animal Models for Evaluation of Oral Delivery of Biopharmaceuticals**

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Abstract

Biopharmaceuticals are increasingly important for patients and the pharmaceutical industry due to their ability to treat and, in some cases, even cure chronic and potentially life-threatening diseases. Most biopharmaceuticals are administered by injection, but intensive focus on development of systems for oral delivery of biopharmaceuticals may result in new treatment modalities to increase patient compliance and reduce product cost.

In the preclinical development phase, use of experimental animal models is essential for evaluation of new formulation designs. In general, limited oral bioavailability of biopharmaceuticals, of just a few percent, is expected, and therefore, the animal models and the experimental settings must be chosen with outmost care. More knowledge and focus on this topic is highly needed, despite experience from the numerous studies evaluating animal models for oral drug delivery of small molecule drugs. This review highlights and discusses pros and cons of the most currently used animal models and settings, and in addition also the influence of anesthetics and sampling methods for evaluation of drug delivery systems for oral delivery of biopharmaceuticals primarily with examples on insulin.

Keywords

Peptides, proteins, insulin, *in situ* perfusion, *in vivo*, macromolecules

Abbreviations: API, active pharmaceutical ingredient; BE, bioequivalence; CLSM, confocal laser scanning microscopy; DDS, drug delivery system; ELISA, enzyme-linked immunosorbent assay; EMA, European Medicines Agency; FDA, U.S. Food & Drug Administration; FITC, fluorescein isothiocyanate; GI, gastrointestinal; GLP1, glucagon-like peptide 1; HPLC, high-performance liquid chromatography; IV, intravenous; IVIVC, *in vitro in vivo* correlations; IVIVR, *in vivo in vitro* relationship; LC-MS, liquid chromatography–mass spectrometry; P_{app} , apparent permeability; P_{eff} , effective permeability; PET, positron-emissions-tomography; QSAR, quantitative structural activity relationship; SC, subcutaneous; SEM, standard error of the mean; SPECT/CT, single-photon emission computed tomography; TEM, transmission electron microscopy

1. Introduction

During the last decades, biopharmaceuticals (e.g. peptides and proteins) have become a growing part of the pharmaceutical industry, and the drugs of choice for treatment of numerous chronic and potentially life-threatening diseases e.g. cancer, inflammatory diseases and diabetes [1,2]. At the time being, subcutaneous or intravenous administration of biopharmaceuticals is still the most widely used route of administration. Currently, approximately 100 biopharmaceutical drug compounds are on the market worldwide, and seven of these are in top 10 of the most selling drugs [3–6]. It is estimated that approximately 270 peptides are currently tested in clinical trials and more than 500 are in preclinical development [5]; numbers providing good indications towards a rapidly growing market. Oral delivery of drugs is the preferred route of dosing due to ease of administration, high patient convenience and thus, compliance and relatively low costs [6,7]. Desmopressin, a synthetic analogue of vasopressin, serves as a positive example of a marketed oral peptide drug formulation, along with promising results for oral delivery of semaglutide, a GLP-1 analogue. But despite these successes, there are many obstacles to deliver biopharmaceuticals in general via the oral route. Among those obstacles are the large molecular size of the drug together with their low stability in biological fluids, mainly caused by enzymatic degradation and low pH in the gastrointestinal (GI) environment. Moreover, biopharmaceuticals are known to have a low permeation across the intestinal mucosa [1,3,5,8–10], resulting in a very low bioavailability after oral dosing [11]. Due to the limited bioavailability, selection of the correct animal model and experimental settings are key elements when evaluating oral delivery of biopharmaceuticals and the appurtenant drug delivery systems (DDS). Furthermore, all experimental variables need to be assessed, including how they can potentially affect the readout of the experiment. A recent review by Sjögren *et al.* [12] addresses the importance of anatomy and physiology variability between various species when conducting animal studies. The aim of the present review is to give some guidelines when conducting animal studies, both *in vivo*, *in situ* and *ex vivo*, to assess the potential of oral DDS containing biopharmaceuticals. The models will be described and discussed including their respective advantages and disadvantages.

In the following, *ex vivo* is defined as studies, where the organs are placed in an external environment, whereas in *in situ* studies, the organ is studied as a whole in the living animal. Furthermore, *in vivo* studies are described, when investigating the biopharmaceutical in the whole living animal. In addition, *in vitro* models, refers to experiments with cells or excised tissue outside their normal biological environment, and these will only briefly be described. For a more detailed review on *in vitro* models, the reader is referred to recent reviews [12,13]. *In silico* modelling will also only be briefly touched upon, as this is excellently addressed in a recent review [14].

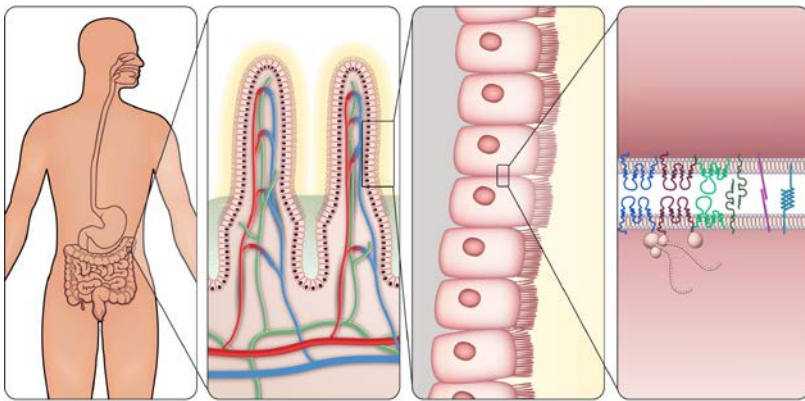
2. Drug delivery system designs for oral delivery of biopharmaceuticals

After almost 100 years of research within the area of oral delivery of biopharmaceuticals [10], more knowledge is still needed to succeed within this topic. As of today, the most promising attempts to succeed with oral delivery of biopharmaceuticals include a combination of enteric coating for delivery to the site of absorption. Moreover, addition of protease inhibitors and permeation enhancers to the DDS may enhance the absorption of the biopharmaceuticals through the intestinal membrane [10]. Novel approaches of utilizing e.g. microneedles in the GI tract may further facilitate the membrane transport [15]. These approaches optimally ensure delivery of an intact drug molecule at or into the surface of the intestinal membrane (the site of absorption), and the transport through the membrane. Delivery of intact and solubilized drug to the site of absorption is challenging due to varying pH in the GI tract, ranging from pH 1–

2 in fasted stomach to pH of 5.5–6.5 in the duodenum, and pH 5.5–7.0 in the large intestine [6]. In both the stomach and intestine, numerous digestive enzymes are present together with an intestinal flora, the microbiota, providing a very unstable environment for the biopharmaceuticals [16]. By utilizing an enteric-coated DDS for protection, it is possible to avoid degradation of the drug and have the biopharmaceutical to pass the stomach and reach the small intestine for absorption. Moreover, it is important to carefully consider the impact of the physicochemical properties, e.g. molecular weight, biophysical stability in the harsh GI environment, lipophilicity and ionization constant of the specific drug for the delivery potential. This needs to be assessed in relation to the biological barriers considering proteolysis in the stomach, variable pH values and poor permeation through the biological membranes, restricting the absorption from the GI tract. It is of course essential to ensure that the biological activity of the biopharmaceutical is maintained when developing an oral DDS [6,17]. The majority of ongoing research includes calcitonin and insulin as model drugs due to their frequent dosing and clinical importance thus, high economic impact [5]. In literature, a variety of *in vivo*, *in situ* and *ex vivo* models have been used involving various animal species, but also many different experimental settings have been utilized [12]. Table 1 and 2 provide an overview of the animal studies in literature with oral DDS for insulin (Table 1) and other biopharmaceuticals (Table 2).

3. Barriers to overcome for successful oral delivery

Apart from preventing degradation, a main obstacle for successful oral delivery of biopharmaceuticals is the limited permeation across the intestinal membrane (Figure 1). Thus, researchers aim to increase the permeation across the biological membrane by various means [3,8,10]. Often, the complexity and variability of the gut physiology and the influence that this may have on absorption is underestimated, when designing DDS to be absorbed from the small intestine. It is essential to include animal studies in the early development phase in order to integrate the dynamic processes happening simultaneously in the body, whereby the iterative design process towards an optimized DDS will have a greater chance of success [18]. Two major determinants for successful absorption from the GI tract are dissolution and permeation, and as biopharmaceuticals are generally freely soluble in aqueous medium with a logP value <0 dissolution will usually not be the rate-limiting step [19,20]. It can therefore be useful to assess the membrane permeability to the given biopharmaceutical *in vitro* before moving to animal models. Examples of *in vitro* permeability experiments include use of excised tissue, cultured cells, artificial membranes and isolated mucosal cells [18,19]. Following positive *in vitro* permeability results, it is essential to perform animal studies. When selecting an animal model, it is important to keep in mind the impact of the anatomical and the physiological differences and similarities between and within species. Even though, the morphology of the intestinal membrane may be seen as comparable in broad terms across species, drug transporter proteins, intestinal metabolizing enzymes, microorganisms, fluid volume and flow, and concentrations of intestinal secretions can differ from species to species, which is crucial to keep in mind [18]. Furthermore, pH values in the stomach and intestine may also differ from the animal in comparison to humans, and the total absorptive area of the intestine is different [12]. In addition, the physiology of the intestine will change with age, and will thus, be different in children and in the elderly population compared to middle-aged adults. This review does not go into depth with the differences in GI physiology, and how it will influence the permeability of intestinal mucosa to oral biopharmaceuticals.



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 140 Figure 1: Graphic showing the *in vivo* barriers in the intestine following oral administration.

Table 1: Overview of studies evaluating oral delivery of insulin in animals

Administration route	Specie	Blood sampling	Quantification method	References
Colonic injection	Rats, diabetic	Portal vein	Blood glucose	[21]
Duodenal administration	Rats	Jugular vein	Blood glucose, ELISA and radioimmunoassay	[7,22–25]
Duodenal cannulation	Rats, diabetic	Carotid artery	Blood glucose	[26]
Duodenal cannulation	Rabbits	Carotid artery	Blood glucose	[27]
<i>Ex vivo</i> ileum	Rabbits	N.S.	P _{app} via HPLC	[28,29]
<i>Ex vivo</i> ileum	Sheep	N.S.	P _{app} via HPLC	[29]
<i>Ex vivo</i> jejunum	Sheep	N.S.	Histology test	[29]
<i>Ex vivo</i> jejunum, duodenum and ileum	Rats	N.S.	HPLC and CLSM	[30–32]
<i>Ex vivo</i> jejunum and colon	Rats	N.S.	Lactate dehydrogenase assay	[33]
<i>Ex vivo</i> permeation of colon	Rats, diabetic	N.S.	HPLC	[21]
<i>In situ</i> duodenal and ileal loop	Rabbits, diabetic	Jugular vein	Blood glucose	[34]
<i>In situ</i> ileal loop perfusion	Rats	Caudal vein	Blood glucose	[35]
<i>In situ</i> isolated intestinal loop	Rats, diabetic	N.S.	Histology of follicular mucosa (Peyer's patches) up to 4 h using fluorescence microscopy	[36]
<i>In situ</i> jejunum, ileum and colon	Rabbits	Mesenteric vein	Radioimmunoassay	[34]
<i>In situ</i> single pass perfusion	Rats	N.S.	HPLC	[37]
	Rats	Jugular vein	Blood glucose, ELISA, PET imaging PET imaging and ELISA	[28,38–41]
Intestinal loop (injection)	Rats	N.S.	Fluorescence microscopy	[31,42,43]
Intraduodenal injection	Rats, diabetic	Tail vein	Blood glucose, enzyme immunoassay kit and blood glucose	[44–46]
Intraduodenal injection	Rats, diabetic	N.S.	Blood glucose	[47]
Intragastric injection	Rats	Tail vein	Blood glucose	[48–50]
Intragastric gavage	Rats, diabetic	Eye	Glucose oxidase and plasma glucose	[51]

Table 1. Continued.

Administration route	Specie	Blood sampling	Quantification method	References
Intragastric gavage	Rats, diabetic	Tail vein	Blood glucose and ELISA	[52–54]
Intragastric gavage	Rats, diabetic	Tail vein	Blood glucose and HPLC	[55]
Intragastric gavage	Rats, diabetic	Leg vein	Blood glucose and ELISA	[56]
Intragastric gavage	Rats, diabetic	Eye	Blood glucose and ELISA	[57]
Intragastric injection	Rats, diabetic	Tail vein	Blood glucose	[50]
Intragastric injection	Mice, diabetic	Tail vein	Blood glucose and ELISA	[58]
Intragastric placement	Pigs	Femoral vein	Blood glucose, ELISA and radiographs	[15]
Intraileal injection	Rats	Tail vein	Blood glucose	[59]
Intrajejunal administration	Rats	Tail or jugular vein	Blood glucose, ELISA and histology	[60]
Intrajejunal injection	Mice	Tail vein	ELISA	[61]
Intrajejunum injection	Pigs	Descending aorta	Blood glucose and ELISA	[62]
Oral administration (tablet, deep in the throat)	Mice, diabetic	Eye	Blood glucose	[63,64]
Oral administration (tablet, deep in the throat)	Rats	Tail vein	Blood glucose and ELISA	[65–69]
Oral administration (tablet)	Rats, diabetic	Tail vein	Blood glucose and ELISA	[70]
Oral gavage (capsules)	Rats, diabetic	Tail vein	Blood glucose and ELISA	[71–77]
Oral gavage (capsules)	Rats, diabetic	N.S.	Blood glucose	[78]
Oral gavage (capsules)	Rats	Tail vein	Blood glucose and ELISA	[30,59,79,80]
Oral gavage (capsules)	Rats, diabetic	Eye	Blood glucose, histology and mucoadhesion	[81]
Oral gavage (capsules)	Rabbits	N.S.	ELISA	[82]
Oral gavage of hydrogel	Rats, diabetic	N.S.	Blood glucose	[83]
Oral gavage of suspension	Mice, diabetic	Tail vein	Blood glucose	[84–86]
Oral gavage of suspension	Mice, diabetic	Eye	Blood glucose and ELISA	[87,88]

Table 1. Continued.

Administration route	Specie	Blood sampling	Quantification method	References
Oral gavage of suspension	Mice	Tail vein	Blood glucose and ELISA	[61,85,89]
Oral gavage of suspension	Rats, diabetic	Eye	Blood glucose, peroxidase, radioimmunoassay, ELISA and CLSM	[33,51,90–104]
Oral gavage of suspension	Rats, diabetic	Tail vein	Blood glucose, ELISA and SPECT/CT	[24,31,36,42,43,72,77,105–125]
Oral gavage of suspension	Rats, diabetic	Femoral artery	Blood glucose and ELISA	[126]
Oral gavage of suspension	Rats	Eye	Blood glucose and ELISA	[127]
Oral gavage of suspension	Rats	Tail vein	Blood glucose, ELISA, imaging and HPLC	[27,106,124,128–130]
Oral gavage of suspension	Rats, diabetic	N.S.	Fluorescence microscopy, CLSM, blood glucose and ELISA	[54,57,131,132]
Oral gavage of suspension	Rats	N.S.	CLSM	[111]
Oral gavage of suspension	Rats	Subclavian vein	Blood glucose and radioimmunoassay	[88,133]
Oral gavage of suspension	Dogs, diabetic	Jugular vein	Blood glucose	[134]
Oral gavage of suspension	Rabbits		Radioimmunoassay	[29]
Oral gavage of suspension	Rabbits, diabetic	Ear vein	Blood glucose	[135]
Oral gavage of suspension	Mice		Imaging via eXplore Optix system	[136]
Oral gavage of suspension	Mice, diabetic	Eye	Blood glucose	[136]

Table 2. Overview of studies evaluating oral delivery of biopharmaceuticals (except for insulin) in animals.

Biopharmaceutical	Administration route	Specie	Blood sampling	Quantification method	References
Antihypertensive peptide (Val-Leu-Pro-Val-Pro-Arg)	Oral gavage of suspension	Rats, hypertensive	N/A	Blood pressure by the tail cuff method	[137]
Antide	Oral administration (tablet, deep in the throat)	Rats	Tail vein	LC-MS of plasma	[138]
Buserelin	Intraduodenal injection	Rats	Carotid artery	Radioimmunoassay	[139]
Exendin-4	<i>In situ</i> perfusion	Rats	Heart puncture	Immunoassay kit	[35,140]
Exendin-4	<i>In situ</i> perfusion	Rats	N.S.	Fluorescence microscopy	[141]
Exendin-4	Intraintestinal injection	Mice, diabetic	Tail vein	Blood glucose	[141]
GLP1	Jejunal placement	Rats	Tail vein	Blood glucose	[49]
GLP1	Oral gavage of suspension	Mice	N.S.	Blood glucose	[142]
GLP1	Oral gavage of suspension	Mice, diabetic	Tail vein	Radioimmunoassay, intraperitoneal glucose tolerance test, blood glucose, near-infrared imaging and X-ray	[143,144]
GLP1	Oral gavage of suspension	Rats	Jugular vein, carotid artery and eye	ELISA	[143,145]
GLP1	Oral gavage of suspension	Rats, diabetic	Tail vein	Blood glucose, ELISA and pancreatic insulin after euthanasia	[146,147]
Granulocyte colony-stimulating factor	Oral gavage of suspension	Rats	Tail vein	ELISA	[148]
Heparin (conjugate)	Oral gavage of suspension	Mice	Heart puncture	Anti-factor assay kit	[149]
Leuprolide	<i>Ex vivo</i> , intestine	Rabbits	N.S.	Radioimmunoassay	[150]
Leuprolide	Intrajejunum, intraileum or intracolonic injection	Rats	Portal vein and aortic artery	Radioimmunoassay	[150]

Table 2. Continued

Biopharmaceutical	Administration route	Specie	Blood sampling	Quantification method	References
Leuprolide	Oral administration (tablet, deep in the throat)	Rats	Tail vein	LC-MS of plasma	[151]
Leuprolide	Oral gavage of suspension	Rats	Tail vein	LC-MS of plasma	[11]
Myrccludex B	Oral gavage of suspension	Rats	Sacrificed	Radioactive liver count	[152]
Protein Alpha crystallin	Oral gavage of suspension	Mice	Eye	ELISA	[153]
Salmon calcitonin	<i>Ex vivo</i> , intestine	Rats	Retroorbital	Fluorescence spectroscopy, ELISA and histology	[154]
Salmon calcitonin	<i>In situ</i> single pass perfusion	Dogs	Portal vein	Radioimmunoassay	[155]
Salmon calcitonin	Intraduodenal injection	Rats	Tail vein	ELISA	[156]
Salmon calcitonin	Intraduodenal injection	Rats	Eye	Colorimetric calcium by UV spectrophotometer	[26]
Salmon calcitonin	Intrajejunal injection	Rats	Tail vein	ELISA	[157]
Salmon calcitonin	Intrajejunal injection	Rats	Heart puncture	Colorimetric method	[158]
Salmon calcitonin	Intrajejunal injection	Rats	Jugular vein	ELISA	[159]
Salmon calcitonin	Oral administration (tablet, deep in the throat)	Rats	Tail vein	Chromogenic assay	[160]
Salmon calcitonin	Oral gavage (capsules)	Rats	Jugular vein	Photometry, radioimmunoassay and	[155,161]
Salmon calcitonin	Oral gavage (capsules)	Rats	Tail vein milking	ELISA	[157]
Salmon calcitonin	Oral gavage of suspension	Rats	Intestinal tissue	CLSM and fluorescence	[162,163]
Salmon calcitonin	Oral gavage of suspension	Rats	Jugular vein	Calcium assay	[163,164]
Salmon calcitonin	Oral gavage of suspension	Rats	Saphenous vein	Calcium assay	[165–167]
Salmon calcitonin	Oral gavage of suspension	Rats	Tail vein	Calcium assay, colorimetric method and ELISA	[168–172]

Abbreviations used in the tables: CLSM: Confocal laser scanning microscopy, ELISA: enzyme-linked immunosorbent assay, HPLC: High-performance liquid chromatography, LC-MS: Liquid chromatography–mass spectrometry, N/A: Not applicable, N.S.: Not stated, UV: ultra-violet.

4. *Ex vivo* and *in situ* models

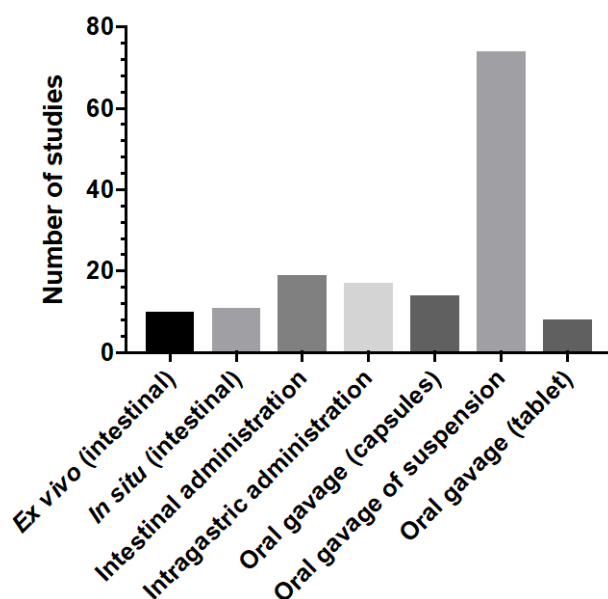
Ex vivo models refer to experiments in live animals with the organs placed in external environments ensuring lowest possible change in native conditions. Similar to studies with *ex vivo* models, *in situ* models may also be used and has the advantage that the whole organ is studied intact in a living animal (Table 3). *Ex vivo* and *in situ* studies count for 14 and 11 % of the total number of conducted animal studies, for studies with insulin (Figure 2A) and other biopharmaceuticals, respectively (Figure 2B) (information from Table 1 and 2). In Figure 2, the *in situ* studies and intestinal administration have been divided into two columns, these can be similar investigations, but the intestinal administration refers to either injection or placement of the DDS in the intestine, whereas the *in situ* studies describes investigations utilizing a flow of medium through the intestinal segment(s). *In situ* perfusion of intestinal segments in the GI tract of rodent, typically rats or alternatively rabbits, are frequently used to study the permeation and absorption kinetics of drugs. Under those experimental settings, intestinal segments can be cannulated and the drug formulation in solution or suspension with or without DDS can be flushed through the isolated intestinal section. This procedure is referred to as the single-pass perfusion model, but as an alternative is the Doluisio approach, a closed-loop model, where the intestinal segment is filled with the solution or suspension throughout the entire experiment [173,174]. Both models have shown to provide intestinal membrane permeability values correlating closely to human data for small molecules [173]. The biggest advantage of the *in situ* methods compared to *in vitro* techniques is the presence of an intact blood and nerve supply in the live animals [18]. Rat and human jejunum effective permeability estimates of passively absorbed drugs in solution correlate highly for small molecules, and both can be used with precision to predict *in vivo* oral absorption of such drugs in man [175].

An advantage with *in situ* perfusion studies is that the whole intestine can be perfused or merely selected small segments, depending on which investigations are initiated. The predictability of the rat *in situ* perfusion model appears to be useful for the prediction of active uptake in humans, as rats have similar patterns of expression of the small intestinal membrane transporters as humans [176]. A recent study used *in situ* closed intestinal loops in rats to identify the region-dependent effect of potential absorption enhancers, penetratin and penetraxin, intended for oral delivery of insulin [40]. The intestinal segments studied were duodenum, jejunum, ileum and colon, and test solutions were administered directly to the loop segments 30 min after surgery. The experiment concluded that ileum and colon appeared to be the most effective target sites for the tested permeation enhancers, as explained by the higher level of protease activity in the upper small intestine [40]. In the same study, it was shown that the maximal absorption detected depended on the enhancer used. Carrier peptides are used in some studies as intestinal absorption enhancers in combination with for example insulin, and for e.g. L-penetratin, the most pronounced effect was observed in the ileum, followed by jejunum, duodenum and colon. In contrast, D-penetratin resulted in the highest blood concentrations of insulin after dosing in the colon, and less after dosing in the duodenum, jejunum and then ileum, respectively [40]. Thus, due to such DDS dependent regional differences, it seems that no general recommendation is clear regarding which region to administer the formulation to. In general, knowledge of GI regional differences related to intestinal drug absorption and effect on the specific evaluated DDS is crucial when setting up an animal experiment. A recent review focused on the intestinal absorption pathways of insulin nanoparticles in animal models [177]. That review concluded that intestinal absorption of insulin-loaded nanoparticles is closely related to accumulation of the particles in Peyer's patches, primarily located in the distal ileum [178], whereas the pathway of delivery for DDS targeting enterocytes and/or tight junctions remains unclear [177].

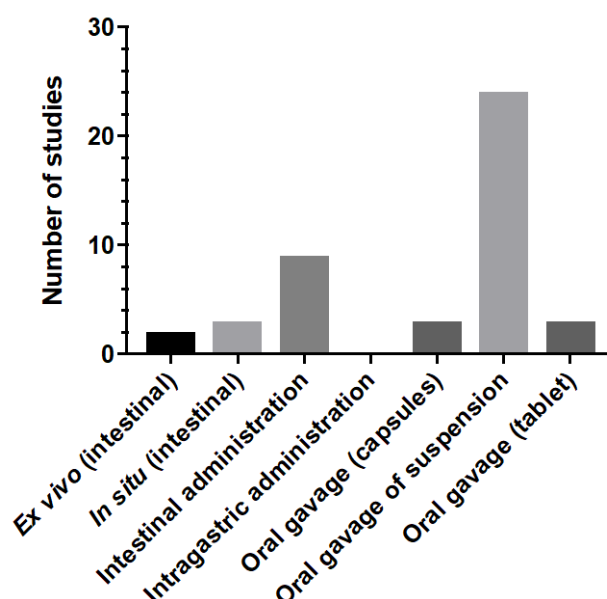
44 *Ex vivo* models are also utilized to investigate membrane permeation of the biopharmaceutical and/or
45 interaction of the DDS with the intestinal membrane. A subcategory of *ex vivo* models is *ex situ* models,
46 where organisms are moved from their natural environment. Often used models in relation to studies on
47 oral delivery of biopharmaceuticals are *ex situ* barrier models assessing transport of compounds across
48 excised intestinal tissue. The use of Ussing chambers to predict oral absorption has previously been
49 reviewed, and the reader is referred to those excellent reviews for more details on the experimental setup
50 [18,179,180]. In the reviews by Sjögren *et al.* [12] and Lennernäs [179], it is highlighted that more
51 knowledge is needed from such *ex vivo* studies especially regarding the regional intestinal effective
52 permeation to form the basis of improved *in silico* models [179]. Since the publication of those reviews, a
53 study has evaluated the permeation of fluorescein isothiocyanate (FITC)-labelled insulin *ex vivo* using fresh
54 rat ileum mucosal tissue and compared the findings to *in vitro* data from Caco-2/HT-29-MTX-E12 cell co-
55 cultures [181]. The study showed that the apparent membrane permeability (P_{app}) of insulin dosed in
56 trimethyl chitosan nanoparticles was 1.34-fold higher compared to unmodified nanoparticles and 1.87-fold
57 increased as compared to the use of micelles [181]. When comparing with *in vitro* data, the same trend was
58 observed both with and without the presence of mucus (e.g. 1.10 vs. 1.16-fold increase with mucus and
59 1.14 vs. 1.23-fold increase without mucus). Last, the study evaluated the DDS in animal studies after oral
60 administration to diabetic rats. The blood glucose depression as observed 3 h after administration was
61 found to be decreased 1.28-fold when comparing trimethyl chitosan nanoparticles to unmodified
62 nanoparticles, whereas the decrease was 1.62-fold when comparing trimethyl chitosan nanoparticles to
63 micelles [181]. Thus, all three models showed the same ranking of the formulations despite more
64 pronounced difference between the formulations in the *in vitro* experiment than in the *in vivo* study. How
65 those data and thus models are related to efficacy studies in man is yet to be addressed.

66 L-valine-appended PLGA particles for oral delivery of insulin has been studied using an *ex vivo* everted
67 intestine method and applied complimentary to oral gavage administration to diabetic rabbits [182,183].
68 The *ex vivo* data showed 48 % insulin transport across the intestine for PLGA particles compared to 91 % for
69 L-valine-appended PLGA after 60 min. When tested in an animal model, the L-valine-appended PLGA
70 showed a slightly sustained hypoglycemic response compared to the non-conjugated particles [183]. Those
71 findings highlight the complexity of relating *ex vivo* data to *in vivo* findings. A more complex barrier must be
72 overcome when administering a formulation orally compared to studying permeation across tissue *ex vivo*,
73 resulting in a less pronounced difference between the DDS tested. Despite the advantage of using animal
74 tissue with functional cells acting as a barrier for drug uptake, such experiments are time consuming to set
75 up, but can be useful for screening and comparing DDS containing the same biopharmaceutical and
76 beneficial to perform prior to *in vivo* studies [18].

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Figure 2: Overview of methods used to evaluate oral bioavailability of insulin (A) and other biopharmaceuticals (B) *in vivo*, *ex vivo* and *in situ* based on reviewed papers listed in Table 1 and 2.

Table 3: Overview of the pros and cons of the most used animal models for testing oral biopharmaceuticals

Model	Aim	Pros	Cons
<i>Ex vivo</i>	Permeation and absorption kinetics	Regional differences can be investigated	Organisms are taken out of the animal
<i>In situ</i>	Permeation and absorption kinetics	Regional differences can be investigated. Permeability data similar to human data	No data on passing through the stomach
<i>In silico</i>	Mechanistic or physiology-based pharmacokinetic simulations	Does not include animals	Does not include <i>in vivo</i> solubility, stability and metabolism
<i>In vivo</i> , healthy animals	Oral PK, PD and bioavailability evaluation	Better animal welfare	Not conclusive to in regards to disease treatment
<i>In vivo</i> , diseased animals	Oral PK, PD, and bioavailability evaluation in diseased animals	Might be a more realistic scenario to the human situation	Large variations in the animal disease and translation of data to man

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5. *In silico* models

In silico approaches refer to computer simulations, ranging from applying simple rules to advanced dynamic modelling [18]. Modelling of compound solubility and membrane permeability plays an increasingly

important role in drug discovery as they can be used as tools for early parameterization of mechanistic or physiology-based pharmacokinetic models or as starting points for refined models of a constrained series of chemical analogues [19,184]. Recently, *in silico* modelling has also been shown to be a useful tool to screen for new permeation enhancers and optimization of the physicochemical aspects of surfactant enhancer systems for oral delivery of proteins [185]. This study utilized a Random Forest Quantitative Structural Activity Relationship (QSAR) model, which was validated based on drug permeation data obtained from studies in Caco-2 cell culture models [185]. It was concluded that this approach serves as a robust strategy to systematically assess novel enhancers, but cannot, however, stand alone in the selection process. As for biopharmaceutical delivery, it is important to emphasize that the model as of today does not include aforementioned important parameters such as solubility, stability and metabolism [185]. A recent and very thorough review did, however, conclude that computational biopharmaceutical profiling is useful for early prediction of drug delivery strategies [14]. For more information on computational prediction, the reader is referred to this review [14].

Several commercial software for advanced *in silico* modelling are available, and three of the most commonly used, Simcyp 13.3, GastroPlus 8.0 and GI-Sim 4.1, were recently compared in relation to their capability to predict human intestinal drug absorption [186]. The study used *a priori* modelling with input data from 12 poorly water soluble drugs, all characterized by incomplete gastrointestinal absorption. It was concluded that the three types of software, all provide useful guidance in formulation development, with GI-Sim and GastroPlus favored over Simcyp due to better prediction of intestinal absorption of incompletely absorbed drugs [186]. Due to the black box nature of *in silico* software, it is generally recommended always to use several models to assess the same problem [12,187]. Moreover, it is very challenging to utilize for biopharmaceuticals due to the complicated degradation kinetics in lumen and during permeation. A highly important aspect to note is that accurate determinations of effective permeability (P_{eff}) is needed to serve as a basis for future *in silico* predictions of oral delivery of biopharmaceuticals [12]. Moreover, it should be emphasized that the current *in silico* models does not include the complex nature of the *in vivo* environments determining the dissolution behavior [188].

6. *In vivo* models

In vivo models comprise the use of living species and in these cases a biopharmaceutical or DDS (containing a biopharmaceutical) are dosed and the effect is tested after appropriate sampling and/or testing. The use of reproducible and reliable *in vivo* models is highly important and required for development and marketing of drugs for oral administration. Biopharmaceuticals are, due to previously described physicochemical properties, characterized by a poor absorption across intestinal epithelium resulting in a very low oral bioavailability, but results from *in vivo* studies highly can depend on the species used [11]. As previously mentioned, it is therefore crucial to utilize a highly sensitive and reproducible model, in order to be able to detect the relatively low changes in pharmacokinetic and pharmacodynamics parameters relating to increased oral bioavailability. Additionally, knowledge about how experimental conditions such as specie morphology, dosing method, anesthesia, sampling method, use of animal disease models resembling human diseases and finally choice of analytical method for sample evaluation is of great importance and will be discussed in the following sections.

6.1. Use of animal models with or without human disease symptoms and choice of specie

One of the first choices to take when conducting animal studies is which specie to choose, and as seen from Figure 3, rats are used in 80 % of the studies listed in Table 1 and 2. Mice represent another species often chosen, used in 11 % of the insulin studies and in 16 % of studies with other biopharmaceuticals. The physiological variations among species were recently reviewed [12], for which reason we will not go into detail with this topic, but rather focus on practical considerations when setting up an animal model. As rats are the most commonly used species in this context, it is important to know the basic differences compared to humans. The GI tract of a rat differs from that of man in several ways with the absence of gall bladder, higher nocturnal activity and different gut flora in the rat. In general, rats appear to provide good estimates for the prediction of absorption for compounds without dissolution problems such as biopharmaceuticals, and also highly reflect the human mucosal barrier in the intestine. Despite this, metabolic differences often lead to misleading predictions of oral bioavailability in humans [18,19].

Generally, when deciding on which animal model to apply, it is important to acknowledge that the bioavailability of biopharmaceuticals will be low even when avoiding the stomach and dosing directly to a specific part of the GI tract, due to enzymatic degradation and poor membrane permeability of large molecules. Bioavailability is, however, found to be slightly higher when drugs are administered directly to the jejunum as compared to other segments of the intestine [5]. One aspect is the low apparent bioavailability; another is the correlation to humans. A comprehensive study compared the absorption of a whole range of small molecule drugs after dosing to the intestine [176]. The study showed that almost no overall correlation exists between oral bioavailability in rat and human ($r^2=0.29$), whereas a correlation exists for intestinal permeability ($r^2=0.8$), both when considering carrier-mediated transport as well as passive diffusion mechanisms [176]. When evaluating the expression level of transporters in duodenum, a moderate correlation ($r^2=0.56$) exists between rat and human [176].

Another aspect to consider is whether to use animal models of human disease or healthy animals. Often the complexity and variability of gut physiology is underestimated, with only one or two variables being considered, this can either be in dosage form design or drug targeting approach [189]. Although strides have been made towards understanding the conditions and mechanisms responsible for absorption from a healthy gut, knowledge in this field is not yet complete. Even more significant is the lack of understanding the GI environment in the diseased state. Functionalized dosage forms cannot be evaluated in a reproducible manner without a comprehensive understanding of the conditions to which they are subjected during *in vivo* testing. Understanding and taking into account the intestinal environment will not only open up for improved evaluation of new dosage form designs, but also improve experimental settings for *in vitro* and pre-clinical tests in animal models leading to better *in vitro in vivo* correlations (IVIVC), and thus, opening new avenues for oral DDS for biopharmaceuticals [189].

When reviewing the existing literature (Figure 3), 63 % of the studies administering insulin (Table 1) have included use of animal models of human diseases, whereas this is only the case for 14 % of non-insulin biopharmaceuticals (Table 2). The overall purpose of insulin administration is to replace the partly or complete lack of insulin in diabetic patients to prevent hyperglycemia [190]. Therefore, animal models of human diseases, in this case diabetic animals, are commonly used in order to gain insight of the efficacy of the administered DDS, eventually combined with knowledge of the mechanistic behavior of DDS [191].

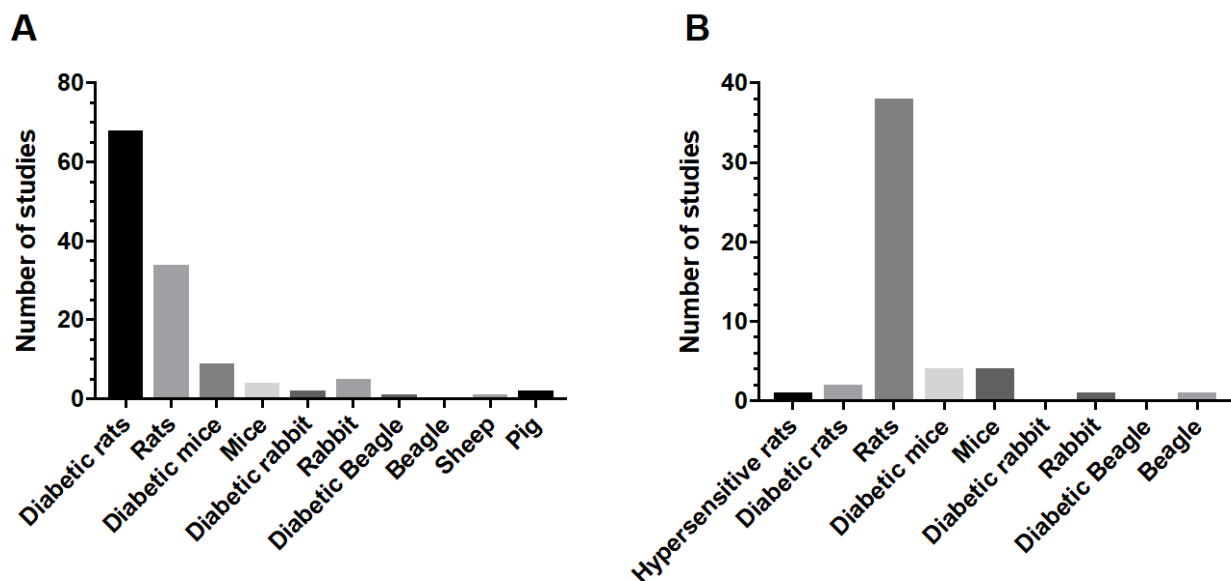


Figure 3: Overview of species used to evaluate oral bioavailability of insulin (A) and other biopharmaceuticals (B) *in vivo*, *in situ* or *ex vivo*. The data are based on reviewed papers, listed in Table 1 and 2.

Numerous diabetic animal models exist, ranging from type 1 diabetic with spontaneously developing autoimmune diabetes, chemical ablation of pancreatic β -cells to type 2 diabetic models, where both obese and non-obese animals are included. Moreover, transgenic and knockout mouse models are also used within diabetic research [190,192]. In the reviewed papers (Table 1), the most commonly used diabetic model is streptozotocin-induced diabetes in rats or mice, done by single intraperitoneal injection of 40-60 mg/kg streptozotocin to rats [77,124] or 65-150 mg/kg to mice [84,87] destroying the pancreatic β -cells [193]. The animals are considered diabetic once the plasma glucose level reaches ≥ 250 mg/dL for rats [77] and ≥ 300 mg/dL to 400 mg/dL for fasted (12 h) and fed mice [84,87]. Unfortunately, streptozotocin does not only harm the pancreatic β -cells [194], but also causes renal injury together with oxidative stress inflammation and endothelial dysfunction [195], which may influence the readout. Thus, as there are pros and cons associated with the various animal models and induction of human diseases in these, careful consideration should be taken to select animal model(s) representing the physiological diversity seen among human diabetic patients [191]. Animal disease models seldom copy all the aspects of the corresponding human disease, and are less characterized in the toxicology area compared to healthy animals. For securing this, several reviews suggests that more than one animal model of human disease should be included in the studies [190,192,196]. However, the exact same aspect of heterogeneity in diabetic expression and complications hereof considerably challenges data evaluation from animal studies, as it might be problematic to separate the drug-induced effect from disease-related complications [191]. Besides the always relevant discussion regarding the use of diseased animal models, it has been discussed that different species and strains behave differently both in relation to induction of diabetes and during treatment hereof [190]. In general, animal models cannot observe the differences seen between diabetic men and women when looking into for example cardiovascular complications [196]. Moreover, animals of different gender e.g. for diabetic rats, might also respond differently to experimentally induced stress and

other metabolic variations, thus leading to gender-biased results. This is not seen in the same way for humans, but can influence the results of the animal studies substantially [190,196].

No clear answer exists to the question of whether to use healthy or diseased animal models. Nonetheless, many caveats are associated with the use of animal models of human disease for assessment of oral DDS, when evaluating biopharmaceuticals with a known mode of action. Also, the animal welfare in terms of the complications associated with models of human diseases such as lack of histology control, diversity in disease expression leading to inclusion of more than one model of human disease, decreased life span and disease-related complications must be carefully considered [191,192].

In terms of species, healthy animals such as Sprague-Dawley rats, CD-1 mice, Beagle dogs, cynomolgus monkeys and mini pigs are the most commonly used models for evaluation of small molecule drugs due to good homogeneity [191]. For biopharmaceuticals, however, a more pronounced species specificity exists [191], as certain biopharmaceuticals are only active when administered to humans or chimpanzees and in other cases immunogenicity hampers full assessment in some species [197]. Such cases and alternative strategies to address such challenges have been thoroughly reviewed previously, for this reason the reader is referred here for further information [197].

6.2. Effect of anesthesia on the readout

Despite common knowledge in the scientific community of the fact that anesthesia is likely to affect the desired readout in animal models, not much literature exists addressing this aspect. When evaluating blood pressure, it is known that determination hereof is easier and with more accurate results when anaesthetizing the animals [198]. Contrary, anesthesia also introduces a significant variable, as it alters the blood pressure and cardiovascular reflexes among other physiological parameters [198].

It has been discussed from an animal welfare perspective and also from a scientific validity perspective within the area of musculoskeletal research that standard protocols for anesthesia and pain management should be developed and applied for animal models [199]. A study from 1983 shows that intraperitoneal injection of pentobarbital to healthy rats increases the blood glucose level by 33 % already 3 min after administration, and returns to normal level only after 40 min [200]. Figure 4 depicts the effect on blood glucose level following subcutaneous (SC) administration of insulin to healthy male Sprague Dawley rats anaesthetized using the most commonly used anesthetics for such studies. The experiments were conducted after 12 h.

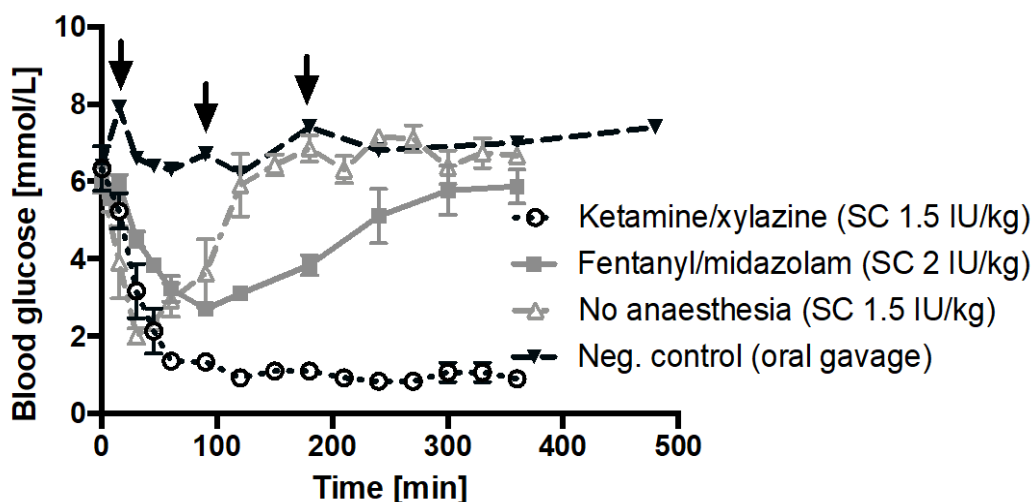


Figure 4: Effect of anesthesia on blood glucose level in healthy rats after subcutaneous (SC) dosing of insulin. The black arrows indicate momentary inhalation of isoflurane. The curves represent the average of three rats \pm SEM, except for the negative control where $n=1$. Blood samples were collected via the sublingual tongue vein.

The data depicted in Figure 4 clearly shows that a combination of ketamine/xylazine significantly decreases the blood glucose level, which is highly problematic if evaluating the unbiased effect of orally administered insulin. Fentanyl/midazolam does not have the same pronounced effect, but still results in a different profile as compared to non-anesthetized animals. More precisely, the maximum effect on the blood glucose level following insulin administration is delayed 60 min in the anaesthetized rats when compared to non-anaesthetized rats, and the recovery period is likewise significantly prolonged. It could be speculated, however, that the reduced recovery period in the non-anesthetized animals when compared to the anaesthetized animals is not only related to the effect of anesthesia, but also the blood sampling procedure. Thus, blood collection via the sublingual tongue causes a stress-induced elevated blood glucose level. Having said that, the authors experienced no sign of stress during handling in terms of diarrhea, urine excretion, screaming, fear of handling upon repeated blood sampling etc., which was the case when repeating the experiment using a restrainer. Conclusively, the effect of anesthesia is the most plausible explanation for variation in blood glucose level.

In the negative control group, the rats were subjected to momentary inhalation of isoflurane (shown by black arrows in Figure 4), and this is shown to increase the blood glucose level, similar to the previously described effect of pentobarbital [200].

Summing up, unless the selected animal model requires rigid restraint or if it is unethical from an animal welfare perspective due to the burden applied to the animal in conscious state after e.g. surgery, it is favored to use conscious models to avoid the impact from anesthesia [198]. Having said that, the stress applied to animals during surgeries such as cannulation of the intestine affects the animal for up to four days after surgery, and therefore, a recovery period of one week is highly recommended before conducting the experiment.

6.3. Routes of administration and practical considerations

259 Choosing the optimal administration route to the animal models requires careful considerations in order to
260 minimize the risk of potential adverse events [201]. Some of the aspects to be considered include the
261 expertise or training required for successful administration, the volume or size of the dosage form needed
262 for administration of a sufficient dose, the precise administration site, pH of the test sample and to which
263 extent animal restraint is needed [201]. When evaluating the effect of orally administered DDS for delivery
264 of biopharmaceuticals, the most frequently used dosing method is by far oral gavage (Table 1 and 2, Figure
265 3).

266 Oral gavage, mimicking the intended route of administration to humans, requires restraint of the animals
267 and correspondingly moderate training of the research personnel [201]. It has been shown that such
268 restraint induces increase in both blood pressure and heart rate for up to 1 h following the dosing with
269 gavage together with an increased stress level for the animals [202]. This can, however, be significantly
270 reduced if practicing the procedure with the animals in advance. For mice, the stress level is already
271 normalized on the second day of training [202], whereas rats requires three training days to maintain
272 normal heart rate and blood pressure during oral gavage [203]. Besides proper training, the stress level
273 associated with oral gavage can be decreased by dipping the gavage device in sucrose before dosing [202].
274 This is, however, not recommended when evaluating compounds such as insulin and GLP-1, where blood
275 glucose level can be the desired readout. Also, soft gavage tubes are favored over stainless steel, as it
276 induces less stress to the animals. Although, a drawback of using soft tubes is the risk of the animals biting
277 the tubes causing even more stress to the animals and potentially exclude the animal from the experiment
278 [201]. Another important aspect to consider is the dosing volume, which is not recommended to exceed 5
279 mL/kg. Larger volumes are likely to induce passive reflux, aspiration pneumonia, irritation in or even
280 rupture of the GI tract [201,204] together with gastric distension, as rodents are not able to vomit [201].
281 Last, the solution or suspension administered should have room temperature not to induce unnecessary
282 stress to the animals.

283 Oral administration of tablets or capsules is an alternative to oral gavage of liquids. As seen from Table 1
284 and 2, tablets are administered by placement in the deep throat thus, activating the swallowing reflex of
285 the animal. The capsules are dosed by utilizing a commercially available steel device for the dosing of the
286 capsules to the stomach. For both tablets and capsules, the size hereof must be scaled to the animal to
287 which it is administered [201]. Although, certain sizes are recommended, it has been shown that enteric-
288 coated capsules of a commercially available size scaled to rats (7.18 mm in length) do not reach the
289 intestine after dosing to rats, but remains in the stomach, where they dissolve [205]. Interestingly, if
290 shortening the capsules to a length of 3.5 mm, they may be emptied from the stomach to the intestine. The
291 study also concluded on a faster gastric emptying and transit of the capsule to the intestine in fed state
292 animals as compared to animals in the fasted state [205]. The potential drawback of using the shortened
293 capsules is a very limited loading capacity and also difficulty in handling the small capsules. Moreover, one
294 should aim for achieving a homogeneous coating of the capsules (or tablets), and avoid scratches in the
295 coating during handling and dosing, as this is likely to significantly impact the *in vivo* faith of the dosage
296 form thus, induce sample variation. Also, powders can be administered via oral gavage, using a positive
297 displacement pipetting device [206].

298 Compared to oral gavage, intragastric and intrainestinal administrations are more invasive procedures
299 requiring surgical skills of the research personnel and also utilization of anesthesia. Nevertheless, when
300 considering the previously mentioned correlation (section 6.1) between bioavailability in rat and human
301 being $r^2=0.29$ and $r^2=0.8$ (after intragastric administration) [176], these methods are highly relevant to

302 consider. Many variations of this procedure exist, including whether the DDS is administered by injection to
303 the absorption site or dosed via an inserted cannula. In addition, the DDS may also be administered to
304 different regions of the intestine and then it is important to consider if the DDS is administered under
305 anesthesia (which is always the case for injections to the GI tract) or after a recovery period in conscious
306 cannulated animals. Regarding the effect of anesthesia, the reader is referred to the discussion in section
307 6.2.

308 For injections or *in situ* studies, the material of the potential cannulas should be carefully considered [207].
309 A recent review provides, a very useful overview of pros and cons of the available materials [207]. In brief,
310 the most important aspects to consider are the biocompatibility, the cannula inner wall diameter (in
311 relation to the DDS administered) and risk of bacterial adherence. Moreover, flexibility of the material and
312 chemical and temperature resistance are also important as a soft material of the cannula is less of a burden
313 for the animal compared to a less flexible material [207]. The parameters are more or less essential
314 depending on the length of the study and if the animals are to recover from surgery for a longer time
315 before the experiment can start, or are anesthetized during the whole study. When working with conscious
316 models, it is important to perform the surgical procedure under as clean conditions as possible, and
317 therefore, autoclaving the cannula can be important [207].

318 Summing up, there are pros and cons for both oral gavage, intragastric or intrainestinal administration.
319 Oral gavage is less invasive and requires moderate training of research personnel, whereas intragastric and
320 intrainestinal administrations are invasive and requires intensive surgical training. Also, taking the one-
321 week recovery period into account, the throughput is lower for intragastric and intrainestinal
322 administrations compared to oral gavage. A significant disadvantage of oral gavage is, however, the very
323 limited correlation to man, whereas a good correlation exists for intragastric administration. This is an
324 important aspect to consider, due to the very limited oral bioavailability of biopharmaceuticals.

325

326 **6.4. Blood sampling methods**

327 When evaluating DDS in animal models, the most common readout is a pharmacological effect or
328 pharmacokinetic profiling, either by quantification of blood glucose after dosing biopharmaceuticals such
329 as insulin and GLP-1 or by compound-specific assays such as enzyme-linked immunosorbent assays (ELISA).
330 Thus, collection of blood samples is essential, and as for all aspects of animal studies, this also involves
331 careful consideration of the advantages and drawbacks of the methods available in order to induce least
332 possible stress to the animals. In Figure 5, the used methods for blood sampling can be observed (compiled
333 from studies reported in Table 1 and 2).

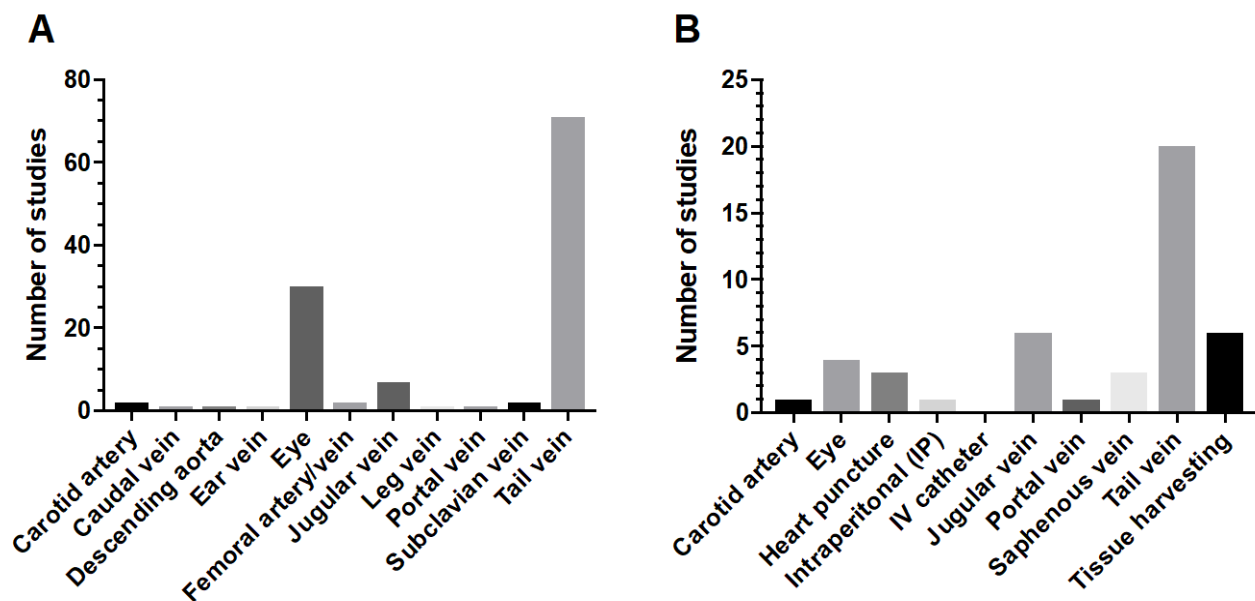


Figure 5: Overview of sampling methods used to evaluate oral bioavailability of insulin (A) and other biopharmaceuticals (B) following *in vivo*, *in situ* or *ex vivo* studies. The graphs are based on the reviewed papers listed in Table 1 and 2.

From Figure 5, it is clear that blood sampling from the tail vein is by far the most commonly used method in mice and rats. However, several methods exist to collect blood from the tail vein [201,208], and it can be performed on the animals either in conscious or anaesthetized state. One approach is to use a restrainer, where the animal enters with their head first and the tail is secured in place by a plug or stopper [207]. For minimizing applying stress to the animals, a red or dark tube is favorable [207], together with frequent washing to avoid cross infection and pheromonal deposition [208]. Once having fixated the rat, the blood can be collected either by vein puncturing using a lancet or needle, or by insertion of a temporary surgical cannula for repeated sample collection. Prior to the sampling, the tail can either be dipped into lukewarm water or placed under a heating lamp to ease access to the tail vein [208], and the blood is typically collected using a capillary tube. An alternative is milking of the tail, where a puncture on the vein is conducted, and the blood is milked out. Here, extreme care must be taken not to rub the tail too intensely, as this may result in leucocytosis and burns. Administration of local analgesic cream prior to sample collection can reduce the stress induced on the animals [208]. Alternative to a restrainer, a towel [207] or even the hands can be used to wrap the animals, keeping the tail free, but whereas the restrainer only requires one person, two persons are needed for these procedures.

Collection of blood from the eye is the second most used blood sampling method for assessment of orally administered biopharmaceuticals (Figure 5). The animals do need to be anaesthetized during blood sampling, and it is not recommended for repeated blood sampling as there is a potential damage of the eye, and in addition also much stress is induced to the animal [208].

For repeated blood sampling, insertion of a cannula should be considered in order to reduce the stress of the animal. According to Figure 5, the jugular vein or alternatively the carotid artery are commonly used in rats, although these methods require intensive surgical training of the research personnel. The surgery is conducted under full anesthesia, and blood samples can be collected in either the anaesthetized or

conscious state. During surgery, the jugular vein or carotid artery is localized, a small incision is made into the vein or artery and the cannula is carefully inserted and securely fastened. For studies with conscious animals, the cannula is tunneled under the skin to exit in the neck and a harness is employed [207,208]. The surgery must be done in a clean environment to avoid infections. The considerations regarding the choice of cannula are as described for intragastric and intrainestinal administrations in section 6.3. When collecting blood, the cannula is flushed with sterile saline added anticoagulant between sample collection, and it is highly important to minimize dilution of the blood by using the lowest possible volume of saline. Heparin and EDTA are the most commonly used anticoagulants, and it is of course important to consider a potential interference of the anticoagulant with the biopharmaceutical in the analytical assay. Blood sampling from the oral cavity or the sublingual tongue vein is also a possibility. This is a fast and easy method, but there is a significant risk of contamination of these samples when the biopharmaceutical is dosed using oral gavage. Moreover, this method can only be conducted in conscious state, and requires restrain of the animals hence, risk of inducing unnecessary stress to the animals.

6.5. Analytical methods

An overview of the analytical methods used after drug administration is given in Figure 6. When evaluating insulin, blood glucose is the most common readout (Figure 6A). Besides, providing information of the pharmacodynamics regarding the effect of the administered biopharmaceutical, it is also a valuable tool to continuously monitor the animal burden while conducting the experiment, and thereby, preventing hypoglycemia in the animals. For testing other biopharmaceuticals than insulin, the preferred analytical method is compound-specific assays such as ELISA and radioimmunoassays providing pharmacokinetic data (Figure 6B), and these methods are often second choice when evaluating insulin-loaded DDS. Supplementary to the aforementioned methods, microscopic and spectroscopic techniques can be used. Here, information regarding deposition and mechanistic behavior of the DDS can be gained. Those methods are usually conducted after euthanasia, and do therefore only provide information for specific time points. Consequently, if using these methods, more animals are used to assess the *in vivo* faith of a DDS over time. Alternative methods such as single photon emission computed tomography/computerized tomography (SPECT/CT) can be considered, and here the labeled DDS is administered via the chosen route of administration, and the *in vivo* faith of the administered sample is followed over time [209]. A significant drawback of this approach is, however, that it requires very expensive equipment and radiolabeling of the test compounds immediately prior to administration. However, the method allows for collection of images of whole animals, the distribution of the label can be quantified, and the method also allows for 3D imaging [209]. Fluorescence detection in animals is also possible, but can be difficult and also demands labeling of the DDS (or biopharmaceutical) with a fluorescence probe [210].

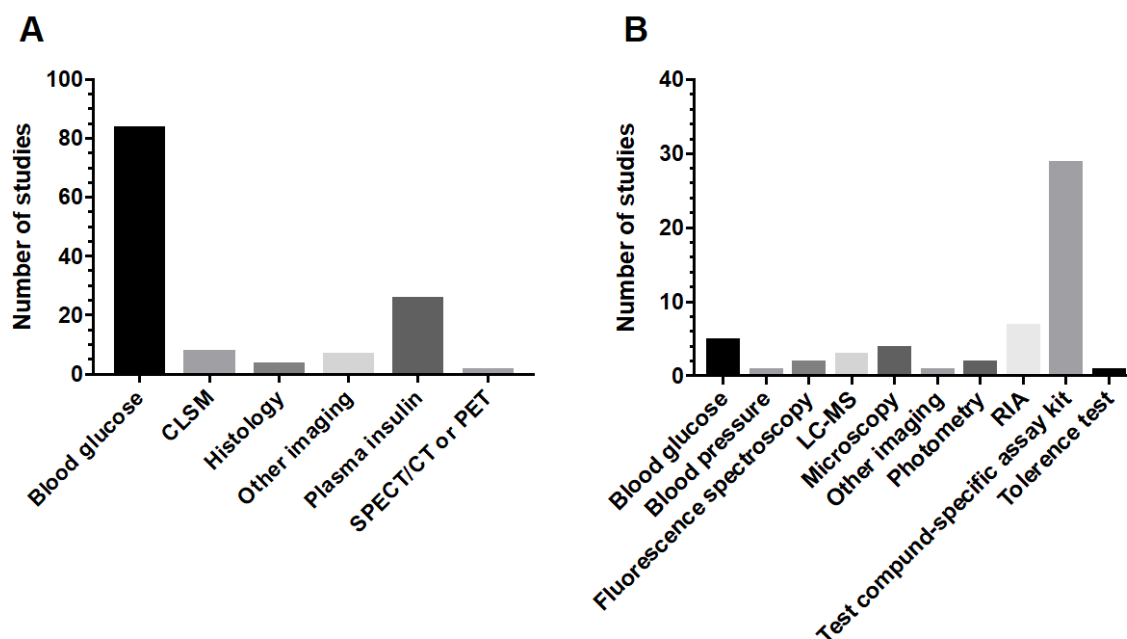


Figure 6:

Overview of the analytical methods used to evaluate oral bioavailability of insulin (A) and other biopharmaceuticals (B) *in vivo*, *in situ* or *ex vivo*. This is based on the reviewed papers listed in Table 1 and 2.

7. Combining and correlating models

IVIVC (also referred to as *in vivo in vitro* relationship) is a major area of interest both for academia and industry, and is included in both the European Medicines Agency (EMA) and the Food & Drug Administration (FDA) guidelines [12]. A recent review by Sjögren *et al.* [12], thoroughly addresses IVIVC and its applications in relation to characterization of DDS, and it will be presented here in brief. IVIVC is mathematically derived as the predicted correlation between *in vitro* dissolution and/or cell models and *in vivo* exposure, yet the term is often used to link *in vitro* behavior to clinical prediction or results [12]. Knowledge about IVIVC is highly important, as it is used for understanding how, and to which extent, changes in the DDS or manufacturing process influence clinical safety and efficacy. Thus, it is a very important tool from an industrial and regulatory perspective, as it is also used as a quality control parameter after product launch [12].

8. Conclusions

Despite the increasing interest in oral delivery of biopharmaceuticals, crucial gaps still exist in relation to knowledge and development of animal models and suitable experimental settings for assessment of biopharmaceuticals dosed by the oral route. As of today, most knowledge of the assessment of oral drugs and the correlation between animal and human studies is based on small molecules. When evaluating orally administered biopharmaceuticals, it is even more crucial to keep in mind that the animal models will merely be models, and as the bioavailability is expected to be very low thorough considerations are essential for all the experimental details, in order to minimize experimental variability and risk of false readouts. This review provides an overview of some of the most important factors influencing the assessment of oral biopharmaceuticals. The review describes the available models and experimental setting used for testing biopharmaceuticals and serves to provide an overview of which animals and methods are

commonly used when testing oral delivery of biopharmaceuticals. Furthermore, it addresses considerations related to use of anesthesia and the effect this can have on the readout of the studies. Likewise, considerations related to blood sampling procedures and analytical methods are discussed in this review. It is impossible to generalize on which models and methods to utilize in specific studies, but this review presents the advantages and disadvantages of the various methods used so far, hence easing the test designs regarding animal models and methods for the evaluation of biopharmaceuticals to be administered by the oral route.

430

431 **Conflicts of interest**

432 None

433

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452 **References**

- 453 [1] J.H. Hamman, G.M. Enslin, A.F. Kotzé, Oral delivery of peptide drugs, *BioDrugs*. 19 (2005) 165–177. doi:10.2165/00063030-200519030-00003.
- 454 [2] Global peptide therapeutics pipeline insight 2015, ID 3096565. (2015).
455 [http://www.researchandmarkets.com/publication/msloabz/global_peptide_therapeutics_pipeline_i](http://www.researchandmarkets.com/publication/msloabz/global_peptide_therapeutics_pipeline_insighGlobal)
456 [nsighGlobal](http://www.researchandmarkets.com/publication/msloabz/global_peptide_therapeutics_pipeline_insighGlobal) (accessed November 1, 2016).
- 457 [3] B.F. Choonara, Y.E. Choonara, P. Kumar, D. Bijukumar, L.C. du Toit, V. Pillay, A review of advanced
458 oral drug delivery technologies facilitating the protection and absorption of protein and peptide
459 molecules, *Biotechnol. Adv.* 32 (2014) 1269–82. doi:10.1016/j.biotechadv.2014.07.006.
- 460 [4] K. Ganguly, K. Chaturvedi, U.A. More, M.N. Nadagouda, T.M. Aminabhavi, Polysaccharide-based
461 micro/nanohydrogels for delivering macromolecular therapeutics, *J. Control. Release*. 193 (2014)
462 162–173. doi:10.1016/j.jconrel.2014.05.014.
- 463 [5] A.L. Smart, S. Gaisford, A.W. Basit, Oral peptide and protein delivery: intestinal obstacles and
464 commercial prospects, *Expert Opin. Drug Deliv.* 11 (2014) 1323–35.
465 doi:10.1517/17425247.2014.917077.
- 466

- 467 [6] J. Renukuntla, A.D. Vadlapudi, A. Patel, S.H.S. Boddu, A.K. Mitra, Approaches for enhancing oral
468 bioavailability of peptides and proteins, *Int. J. Pharm.* 447 (2013) 75–93.
469 doi:10.1016/j.ijpharm.2013.02.030.
- 470 [7] P.L. Lam, R. Gambari, Advanced progress of microencapsulation technologies: In vivo and in vitro
471 models for studying oral and transdermal drug deliveries, *J. Control. Release.* 178 (2014) 25–45.
472 doi:10.1016/j.jconrel.2013.12.028.
- 473 [8] S.R. Hwang, Y. Byun, Advances in oral macromolecular drug delivery, *Expert Opin. Drug Deliv.* 11
474 (2014) 1–13. doi:10.1517/17425247.2014.945420.
- 475 [9] P. Colombo, F. Sonvico, G. Colombo, R. Bettini, Novel platforms for oral drug delivery, *Pharm. Res.*
476 26 (2009) 601–611. doi:10.1007/s11095-008-9803-0.
- 477 [10] E. Moroz, S. Matoori, J.C. Leroux, Oral delivery of macromolecular drugs: Where we are after almost
478 100years of attempts, *Adv. Drug Deliv. Rev.* 101 (2016) 108–121. doi:10.1016/j.addr.2016.01.010.
- 479 [11] J. Iqbal, G. Shahnaz, G. Perera, F. Hintzen, F. Sarti, A. Bernkop-Schnürch, Thiolated chitosan:
480 development and in vivo evaluation of an oral delivery system for leuprolide, *Eur. J. Pharm.*
481 *Biopharm.* 80 (2012) 95–102. doi:10.1016/j.ejpb.2011.09.010.
- 482 [12] E. Sjögren, B. Abrahamsson, P. Augustijns, D. Becker, M.B. Bolger, M. Brewster, J. Brouwers, T.
483 Flanagan, M. Harwood, C. Heinen, R. Holm, H.P. Juretschke, M. Kubbinga, A. Lindahl, V. Lukacova, U.
484 Münster, S. Neuhoff, M.A. Nguyen, A. Van Peer, C. Reppas, A.R. Hodgegan, C. Tannergren, W.
485 Weitschies, C. Wilson, P. Zane, H. Lennernäs, P. Langguth, In vivo methods for drug absorption -
486 Comparative physiologies, model selection, correlations with in vitro methods (IVIVC), and
487 applications for formulation/API/excipient characterization including food effects, *Eur. J. Pharm. Sci.*
488 57 (2014) 99–151. doi:10.1016/j.ejps.2014.02.010.
- 489 [13] J.M. Gamboa, K.W. Leong, In vitro and in vivo models for the study of oral delivery of nanoparticles,
490 *Adv. Drug Deliv. Rev.* 65 (2013) 800–810. doi:10.1016/j.addr.2013.01.003.
- 491 [14] C.A.S. Bergström, W.N. Charman, C.J.H. Porter, Computational prediction of formulation strategies
492 for beyond-rule-of-5 compounds, *Adv. Drug Deliv. Rev.* 101 (2016) 6–21.
493 doi:10.1016/j.addr.2016.02.005.
- 494 [15] G. Traverso, C.M. Schoellhammer, A. Schroeder, R. Maa, G.Y. Lauwers, B.E. Polat, D.G. Anderson, D.
495 Blankschtein, R. Langer, Microneedles for drug delivery via the gastrointestinal tract, *J. Pharm. Sci.*
496 104 (2015) 362–367. doi:10.1002/jps.24182.
- 497 [16] V.F. Patel, F. Liu, M.B. Brown, Advances in oral transmucosal drug delivery, *J. Control. Release.* 153
498 (2011) 106–116. doi:10.1016/j.jconrel.2011.01.027.
- 499 [17] M. Morishita, N.A. Peppas, Is the oral route possible for peptide and protein drug delivery?, *Drug*
500 *Discov. Today.* 11 (2006) 905–10. doi:10.1016/j.drudis.2006.08.005.
- 501 [18] F. Antunes, F. Andrade, D. Ferreira, H.M. Nielsen, B. Sarmiento, Models to predict intestinal
502 absorption of therapeutic peptides and proteins, *Curr. Drug Metab.* 14 (2013) 4–20.
503 doi:10.2174/138920013804545160.
- 504 [19] N. Fotaki, Pros and cons of methods used for the prediction of oral drug absorption, *Expert Rev. Clin.*
505 *Pharmacol.* 2 (2009) 195–208. doi:10.1586/17512433.2.2.195.
- 506 [20] G. Camenisch, J. Alsenz, H. Van De Waterbeemd, G. Folkers, Estimation of permeability by passive
507 diffusion through Caco-2 cell monolayers using the drugs' lipophilicity and molecular weight, *Eur. J.*
508 *Pharm. Sci.* 6 (1998) 313–319. doi:10.1016/S0928-0987(97)10019-7.
- 509 [21] A. Bayat, F.A. Dorkoosh, A.R. Dehpour, L. Moezi, B. Larijani, H.E. Junginger, M. Rafiee-Tehrani,
510 Nanoparticles of quaternized chitosan derivatives as a carrier for colon delivery of insulin: Ex vivo
511 and in vivo studies, *Int. J. Pharm.* 356 (2008) 259–266. doi:10.1016/j.ijpharm.2007.12.037.
- 512 [22] E. Déat-Lainé, V. Hoffart, G. Garrait, J.F. Jarrige, J.M. Cardot, M. Subirade, E. Beyssac, Efficacy of
513 mucoadhesive hydrogel microparticles of whey protein and alginate for oral insulin delivery, *Pharm.*
514 *Res.* 30 (2013) 721–734. doi:10.1007/s11095-012-0913-3.
- 515 [23] L. Hovgaard, H. Jacobs, D.E. Wilson, S.W. Kim, Stabilization of insulin by alkylmaltosides. B. Oral
516 absorption in vivo in rats, *Int. J. Pharm.* 132 (1996) 115–121. doi:10.1016/0378-5173(95)04414-0.

- 517 [24] K. Sonaje, Y.-H. Lin, J.-H. Juang, S.-P. Wey, C.-T. Chen, H.-W. Sung, In vivo evaluation of safety and
518 efficacy of self-assembled nanoparticles for oral insulin delivery, *Biomaterials*. 30 (2009) 2329–39.
519 doi:10.1016/j.biomaterials.2008.12.066.
- 520 [25] M. Trotta, M.E. Carlotti, M. Gallarate, G.P. Zara, E. Muntoni, L. Battaglia, Insulin-loaded SLN
521 prepared with the emulsion dilution technique: In vivo tracking of nanoparticles after oral
522 administration to rats, *J. Dispers. Sci. Technol.* 32 (2011) 1041–1045.
523 doi:10.1080/01932691.2010.488497.
- 524 [26] N. Li, X.-R. Li, Y.-X. Zhou, W.-J. Li, Y. Zhao, S.-J. Ma, J.-W. Li, Y.-J. Gao, Y. Liu, X.-L. Wang, D.-D. Yin, The
525 use of polyion complex micelles to enhance the oral delivery of salmon calcitonin and transport
526 mechanism across the intestinal epithelial barrier, *Biomaterials*. 33 (2012) 8881–92.
527 doi:10.1016/j.biomaterials.2012.08.047.
- 528 [27] M. Niu, Y. Tan, P. Guan, L. Hovgaard, Y. Lu, J. Qi, R. Lian, X. Li, W. Wu, Enhanced oral absorption of
529 insulin-loaded liposomes containing bile salts: A mechanistic study, *Int. J. Pharm.* 460 (2014) 119–
530 130. doi:10.1016/j.ijpharm.2013.11.028.
- 531 [28] Y. Zhang, X. Lin, X. Du, S. Geng, H. Li, H. Sun, X. Tang, W. Xiao, pH-sensitive thiolated nanoparticles
532 facilitate the oral delivery of insulin in vitro and in vivo, *J. Nanoparticle Res.* 17 (2015) 1–11.
533 doi:10.1007/s11051-014-2847-7.
- 534 [29] A.M.M. Sadeghi, M.R. Avadi, S. Ejtemaimehr, S. Abashzadeh, A. Partoazar, F. Dorkoosh, M. Faghihi,
535 M. Rafiee-Tehrani, H.E. Junginger, Development of a gas empowered drug delivery system for
536 peptide delivery in the small intestine, *J. Control. Release*. 134 (2009) 11–17.
537 doi:10.1016/j.jconrel.2008.10.012.
- 538 [30] L. Yin, J. Ding, L. Fei, M. He, F. Cui, C. Tang, C. Yin, Beneficial properties for insulin absorption using
539 superporous hydrogel containing interpenetrating polymer network as oral delivery vehicles, *Int. J.*
540 *Pharm.* 350 (2008) 220–229. doi:10.1016/j.ijpharm.2007.08.051.
- 541 [31] X. Li, S. Guo, C. Zhu, Q. Zhu, Y. Gan, J. Rantanen, U.L. Rahbek, L. Hovgaard, M. Yang, Intestinal
542 mucosa permeability following oral insulin delivery using core shell corona nanolipoparticles,
543 *Biomaterials*. 34 (2013) 9678–9687. doi:10.1016/j.biomaterials.2013.08.048.
- 544 [32] G. Sandri, M.C. Bonferoni, S. Rossi, F. Ferrari, C. Boselli, C. Caramella, Insulin-loaded nanoparticles
545 based on N-trimethyl chitosan: in vitro (Caco-2 model) and ex vivo (excised rat jejunum, duodenum,
546 and ileum) evaluation of penetration enhancement properties, *AAPS PharmSciTech.* 11 (2010) 362–
547 71. doi:10.1208/s12249-010-9390-3.
- 548 [33] A. Verma, S. Sharma, P.K. Gupta, A. Singh, B.V. Teja, P. Dwivedi, G.K. Gupta, R. Trivedi, P.R. Mishra,
549 Vitamin B12 functionalized layer by layer calcium phosphate nanoparticles: A mucoadhesive and pH
550 responsive carrier for improved oral delivery of insulin, *Acta Biomater.* 31 (2016) 288–300.
551 doi:10.1016/j.actbio.2015.12.017.
- 552 [34] A. Fasano, S. Uzzau, Modulation of intestinal tight junctions by zonula occludens toxin permits
553 enteral administration of insulin and other macromolecules in an animal model, *J. Clin. Invest.* 99
554 (1997) 1158–1164. doi:10.1172/JCI119271.
- 555 [35] H. He, J. Sheng, A.E. David, Y.M. Kwon, J. Zhang, Y. Huang, J. Wang, V.C. Yang, The use of low
556 molecular weight protamine chemical chimera to enhance monomeric insulin intestinal absorption,
557 *Biomaterials*. 34 (2013) 7733–7743. doi:10.1016/j.biomaterials.2013.06.047.
- 558 [36] C. Damgé, P. Maincent, N. Ubrich, Oral delivery of insulin associated to polymeric nanoparticles in
559 diabetic rats, *J. Control. Release*. 117 (2007) 163–170. doi:10.1016/j.jconrel.2006.10.023.
- 560 [37] K. Iwanaga, S. Ono, K. Narioka, M. Kakemi, K. Morimoto, S. Yamashita, Y. Namba, O. Naoto,
561 Application of surface-coated liposomes for oral delivery of peptide: Effects of coating the
562 liposome's surface on the GI transit of insulin, *J. Pharm. Sci.* 88 (1999) 248–252.
563 doi:10.1021/js980235x.
- 564 [38] J. Shimoda, H. Onishi, Y. Machida, Bioadhesive characteristics of chitosan microspheres to the
565 mucosa of rat small intestine, *Drug Dev. Ind. Pharm.* 27 (2001) 567–76. doi:10.1081/DDC-
566 100105182.

- 567 [39] A. Tuesca, K. Nakamura, M. Morishita, J. Joseph, N. Peppas, A. Lowman, Complexation hydrogels for
568 oral insulin delivery: Effects of polymer dosing on in vivo efficacy, J. Pharm. Sci. 97 (2008) 2607–
569 2618. doi:10.1002/jps.21184.
- 570 [40] E.-S. Khafagy, R. Iwamae, N. Kamei, M. Takeda-Morishita, Region-dependent role of cell-penetrating
571 peptides in insulin absorption across the rat small intestinal membrane, AAPS J. 17 (2015) 1427–
572 1437. doi:10.1208/s12248-015-9804-y.
- 573 [41] N. Kamei, M. Morishita, Y. Kanayama, K. Hasegawa, M. Nishimura, E. Hayashinaka, Y. Wada, Y.
574 Watanabe, K. Takayama, Molecular imaging analysis of intestinal insulin absorption boosted by cell-
575 penetrating peptides by using positron emission tomography, J. Control. Release. 146 (2010) 16–22.
576 doi:10.1016/j.jconrel.2010.05.004.
- 577 [42] N. Ahmad, M.C.I. Mohd Amin, I. Ismail, F. Buang, Enhancement of oral insulin bioavailability: *in vitro*
578 and *in vivo* assessment of nanoporous stimuli-responsive hydrogel microparticles, Expert Opin. Drug
579 Deliv. 13 (2016) 621–632. doi:10.1517/17425247.2016.1160889.
- 580 [43] Y. Jin, Y. Song, X. Zhu, D. Zhou, C. Chen, Z. Zhang, Y. Huang, Goblet cell-targeting nanoparticles for
581 oral insulin delivery and the influence of mucus on insulin transport, Biomaterials. 33 (2012) 1573–
582 1582. doi:10.1016/j.biomaterials.2011.10.075.
- 583 [44] A. Kadir, M.T.M. Mokhtar, T.W. Wong, Nanoparticulate assembly of mannuronic acid- and guluronic
584 acid-rich alginate: Oral insulin carrier and glucose binder, J. Pharm. Sci. 102 (2013) 4353–4363.
585 doi:10.1002/jps.23742.
- 586 [45] N. Reix, A. Parat, E. Seyfritz, R. Van Der Werf, V. Epure, N. Ebel, L. Danicher, E. Marchioni, N.
587 Jeandidier, M. Pinget, Y. Frère, S. Sigrist, In vitro uptake evaluation in Caco-2 cells and in vivo results
588 in diabetic rats of insulin-loaded PLGA nanoparticles, Int. J. Pharm. 437 (2012) 213–220.
589 doi:10.1016/j.ijpharm.2012.08.024.
- 590 [46] Z.H. Zhang, Y.L. Zhang, J.P. Zhou, H.X. Lv, Solid lipid nanoparticles modified with stearic acid-
591 octaarginine for oral administration of insulin, Int. J. Nanomedicine. 7 (2012) 3333–3339.
592 doi:10.2147/IJN.S31711.
- 593 [47] M. Diop, N. Auberval, A. Viciglio, A. Langlois, W. Bietiger, C. Mura, C. Peronet, A. Bekel, D. Julien
594 David, M. Zhao, M. Pinget, N. Jeandidier, C. Vauthier, E. Marchioni, Y. Frere, S. Sigrist, Design,
595 characterisation, and bioefficiency of insulin-chitosan nanoparticles after stabilisation by freeze-
596 drying or cross-linking, Int. J. Pharm. 491 (2015) 402–408. doi:10.1016/j.ijpharm.2015.05.065.
- 597 [48] F. Cui, F. Qian, Z. Zhao, L. Yin, C. Tang, C. Yin, Preparation, characterization, and oral delivery of
598 insulin loaded carboxylated chitosan grafted poly(methyl methacrylate) nanoparticles,
599 Biomacromolecules. 10 (2009) 1253–1258. doi:10.1021/bm900035u.
- 600 [49] V. Gupta, B.H. Hwang, N. Doshi, A. Banerjee, A.C. Anselmo, S. Mitragotri, Delivery of exenatide and
601 insulin using mucoadhesive intestinal devices, Ann. Biomed. Eng. 44 (2016) 1–15.
602 doi:10.1007/s10439-016-1558-x.
- 603 [50] F. Cui, F. Qian, Z. Zhao, L. Yin, C. Tang, C. Yin, Preparation, characterization, and oral delivery of
604 insulin loaded carboxylated chitosan grafted poly(methyl methacrylate) nanoparticles,
605 Biomacromolecules. 10 (2009) 1253–1258. doi:10.1021/bm900035u.
- 606 [51] S. Sun, N. Liang, Y. Kawashima, D. Xia, F. Cui, Hydrophobic ion pairing of an insulin-sodium
607 deoxycholate complex for oral delivery of insulin, Int. J. Nanomedicine. 6 (2011) 3049–3056.
608 doi:10.2147/IJN.S26450.
- 609 [52] B. Sarmiento, S. Martins, Oral insulin delivery by means of solid lipid nanoparticles, 2 (2007) 743–
610 749. doi:10.1177/193229681300700228.
- 611 [53] B. Sarmiento, A. Ribeiro, F. Veiga, P. Sampaio, R. Neufeld, D. Ferreira, Alginate/chitosan
612 nanoparticles are effective for oral insulin delivery, Pharm. Res. 24 (2007) 2198–2206.
613 doi:10.1007/s11095-007-9367-4.
- 614 [54] B. Sarmiento, A. Ribeiro, F. Veiga, D. Ferreira, R. Neufeld, Oral bioavailability of insulin contained in
615 polysaccharide nanoparticles, Biomacromolecules. 8 (2007) 3054–3060. doi:10.1021/bm0703923.
- 616 [55] P. Fonte, T. Nogueira, C. Gehm, D. Ferreira, B. Sarmiento, Chitosan-coated solid lipid nanoparticles

enhance the oral absorption of insulin, *Drug Deliv. Transl. Res.* 1 (2011) 299–308. doi:10.1007/s13346-011-0023-5.

[56] A. Graf, T. Rades, S.M. Hook, Oral insulin delivery using nanoparticles based on microemulsions with different structure-types: Optimisation and in vivo evaluation, *Eur. J. Pharm. Sci.* 37 (2009) 53–61. doi:10.1016/j.ejps.2008.12.017.

[57] P. Hurkat, A. Jain, A. Jain, S. Shilpi, A. Gulbake, S.K. Jain, Concanavalin A conjugated biodegradable nanoparticles for oral insulin delivery, *J. Nanoparticle Res.* 14 (2012) 1219. doi:10.1007/s11051-012-1219-4.

[58] P. Mukhopadhyay, P.P. Kundu, Chitosan-graft-PAMAM–alginate core–shell nanoparticles: a safe and promising oral insulin carrier in an animal model, *RSC Adv.* 5 (2015) 93995–94007. doi:10.1039/C5RA17729D.

[59] L. Yin, J. Ding, C. He, L. Cui, C. Tang, C. Yin, Drug permeability and mucoadhesion properties of thiolated trimethyl chitosan nanoparticles in oral insulin delivery, *Biomaterials.* 30 (2009) 5691–5700. doi:10.1016/j.biomaterials.2009.06.055.

[60] K. Whitehead, Z. Shen, S. Mitragotri, Oral delivery of macromolecules using intestinal patches: Applications for insulin delivery, *J. Control. Release.* 98 (2004) 37–45. doi:10.1016/j.jconrel.2004.04.013.

[61] E.J.B. Nielsen, S. Yoshida, N. Kamei, R. Iwamae, E.S. Khafagy, J. Olsen, U.L. Rahbek, B.L. Pedersen, K. Takayama, M. Takeda-Morishita, In vivo proof of concept of oral insulin delivery based on a co-administration strategy with the cell-penetrating peptide penetratin, *J. Control. Release.* 189 (2014) 19–24. doi:10.1016/j.jconrel.2014.06.022.

[62] C.J. Kirby, Oil-based formulations for oral delivery of therapeutic peptides, *J. Liposome Res.* 10 (2000) 391–407. doi:10.3109/08982100009031106.

[63] P. Calceti, S. Salmaso, G. Walker, A. Bernkop-Schnürch, Development and in vivo evaluation of an oral insulin-PEG delivery system, *Eur. J. Pharm. Sci.* 22 (2004) 315–323. doi:10.1016/j.ejps.2004.03.015.

[64] M.K. Marschütz, P. Caliceti, A. Bernkop-Schnürch, Design and in vivo evaluation of an oral delivery system for insulin, *Pharm. Res.* 17 (2000) 1468–1474. doi:10.1023/A:1007696723125.

[65] M. Werle, B. Loretz, D. Entstrasser, F. Föger, Design and evaluation of a chitosan-aprotinin conjugate for the peroral delivery of therapeutic peptides and proteins susceptible to enzymatic degradation, *J. Drug Target.* 15 (2007) 327–333. doi:10.1080/10611860701349141.

[66] B. Deutel, M. Greindl, M. Thaurer, A. Bernkop-Schnürch, Novel insulin thiomers nanoparticles: In vivo evaluation of an oral drug delivery system, *Biomacromolecules.* 9 (2008) 278–285. doi:10.1021/bm700916h.

[67] G. Millotti, F. Laffleur, G. Perera, C. Vigl, K. Pickl, F. Sinner, A. Bernkop-Schnürch, In vivo evaluation of thiolated chitosan tablets for oral insulin delivery, *J. Pharm. Sci.* 103 (2014) 3165–3170. doi:10.1002/jps.24102.

[68] A.H. Krauland, D. Guggi, A. Bernkop-Schnürch, Oral insulin delivery: The potential of thiolated chitosan-insulin tablets on non-diabetic rats, *J. Control. Release.* 95 (2004) 547–555. doi:10.1016/j.jconrel.2003.12.017.

[69] V. Grabovac, F. Föger, A. Bernkop-Schnürch, Design and in vivo evaluation of a patch system based on thiolated polymers, *Int. J. Pharma.* 348 (2008) 169–174. doi:10.1016/j.ijpharm.2007.06.052.

[70] A. Maroni, M. Dorly, D. Curto, S. Salmaso, L. Zema, A. Melocchi, P. Caliceti, A. Gazzaniga, In vitro and in vivo evaluation of an oral multiple-unit formulation for colonic delivery of insulin, *Eur. J. Pharm. Biopharm.* 108 (2016) 76–82. doi:10.1016/j.ejpb.2016.08.002.

[71] M.A. Momoh, F.C. Kenechukwu, P.O. Nnamani, J.C. Umetiti, Influence of magnesium stearate on the physicochemical and pharmacodynamic characteristics of insulin-loaded Eudragit entrapped mucoadhesive microspheres, *Drug Deliv.* 7544 (2014) 1–12. doi:10.3109/10717544.2014.898108.

[72] Z.I. Al-Kurdi, B.Z. Chowdhry, S.A. Leharne, N.A. Qinna, M.M.H. Al Omari, A.A. Badwan, Influence of glucosamine on the bioactivity of insulin delivered subcutaneously and in an oral nanodelivery

- system, *Drug Des. Devel. Ther.* 9 (2015) 6167–6176. doi:10.2147/DDDT.S91974.
- [73] F. Yu, Y. Li, C.S. Liu, Q. Chen, G.H. Wang, W. Guo, X.E. Wu, D.H. Li, W.D. Wu, X.D. Chen, Enteric-coated capsules filled with mono-disperse micro-particles containing PLGA-lipid-PEG nanoparticles for oral delivery of insulin, *Int. J. Pharm.* 484 (2015) 181–191. doi:10.1016/j.ijpharm.2015.02.055.
- [74] S. Abbad, Z. Zhang, A.Y. Waddad, W.L.L. Munyendo, H. Lv, J. Zhou, Chitosan-modified cationic amino acid nanoparticles as a novel oral delivery system for insulin, *J. Biomed. Nanotechnol.* 11 (2015) 486–499. doi:10.1166/jbn.2015.1924.
- [75] K.H. Leong, L.Y. Chung, M.I. Noordin, Y. Onuki, M. Morishita, K. Takayama, Lectin-functionalized carboxymethylated kappa-carrageenan microparticles for oral insulin delivery, *Carbohydr. Polym.* 86 (2011) 555–565. doi:10.1016/j.carbpol.2011.04.070.
- [76] L. Zhang, Z. Zhang, N. Li, N. Wang, Y. Wang, S. Tang, L. Xu, Y. Ren, Synthesis and evaluation of a novel β -cyclodextrin derivative for oral insulin delivery and absorption, *Int. J. Biol. Macromol.* 61 (2013) 494–500. doi:10.1016/j.ijbiomac.2013.08.034.
- [77] Z. Wu, L. Ling, L. Zhou, X. Guo, W. Jiang, Y. Qian, K. Luo, L. Zhang, Novel preparation of PLGA/HP55 nanoparticles for oral insulin delivery, *Nanoscale Res. Lett.* 7 (2012) 299. doi:10.1186/1556-276X-7-299.
- [78] B. D'Souza, T. Bhowmik, M.N. Uddin, C. Oettinger, M. D'Souza, Development of β -cyclodextrin-based sustained release microparticles for oral insulin delivery, *Drug Dev. Ind. Pharm.* 40 (2014) 9045 (2014) 1–6. doi:10.3109/03639045.2014.947507.
- [79] M. Licciardi, G. Pitarresi, G. Cavallaro, G. Giammona, Nanoaggregates based on new poly-hydroxyethyl-aspartamide copolymers for oral insulin absorption, *Mol. Pharm.* 10 (2013) 1644–1654. doi:10.1021/mp300226d.
- [80] L. Yin, J. Ding, J. Zhang, C. He, C. Tang, C. Yin, Polymer integrity related absorption mechanism of superporous hydrogel containing interpenetrating polymer networks for oral delivery of insulin, *Biomaterials.* 31 (2010) 3347–3356. doi:10.1016/j.biomaterials.2010.01.045.
- [81] Y. Zhang, X. Wu, L. Meng, Y. Zhang, R. Ai, N. Qi, H. He, H. Xu, X. Tang, Thiolated Eudragit nanoparticles for oral insulin delivery: Preparation, characterization and in vivo evaluation, *Int. J. Pharm.* 436 (2012) 341–350. doi:10.1016/j.ijpharm.2012.06.054.
- [82] V. Uskokovi, Shape effect in the design of nanowire-coated microparticles as transepithelial drug delivery devices, *ACS Nano.* 6 (2012) 7832–7841. doi:10.1021/nn3019865.
- [83] S. Park, Y. Nho, Y. Lim, H. Kim, Preparation of pH-sensitive poly (vinyl alcohol-g-methacrylic acid) and poly (vinyl alcohol-g-acrylic acid) hydrogels by gamma ray irradiation and their insulin release behavior, *J. Appl. Polym. Sci.* 91 (2004) 636–643.
- [84] Y. Dekel, Y. Glucksam, R. Margalit, Novel fibrillar insulin formulations for oral administration: Formulation and in vivo studies in diabetic mice, *J. Control. Release.* 143 (2010) 128–135. doi:10.1016/j.jconrel.2009.12.018.
- [85] X.Y. Xiong, Q.H. Li, Y.P. Li, L. Guo, Z.L. Li, Y.C. Gong, Pluronic P85/poly(lactic acid) vesicles as novel carrier for oral insulin delivery, *Colloids Surfaces B Biointerfaces.* 111 (2013) 282–288. doi:10.1016/j.colsurfb.2013.06.019.
- [86] P. Mukhopadhyay, K. Sarkar, M. Chakraborty, S. Bhattacharya, R. Mishra, P.P. Kundu, Oral insulin delivery by self-assembled chitosan nanoparticles: In vitro and in vivo studies in diabetic animal model, *Mater. Sci. Eng. C.* 33 (2013) 376–382. doi:10.1016/j.msec.2012.09.001.
- [87] S. Salmaso, S. Bersani, N. Elvassore, A. Bertucco, P. Caliceti, Biopharmaceutical characterisation of insulin and recombinant human growth hormone loaded lipid submicron particles produced by supercritical gas micro-atomisation, *Int. J. Pharm.* 379 (2009) 51–58. doi:10.1016/j.ijpharm.2009.06.014.
- [88] N. Zhang, Q.N. Ping, G.H. Huang, W.F. Xu, Investigation of lectin-modified insulin liposomes as carriers for oral administration, *Int. J. Pharm.* 294 (2005) 247–259. doi:10.1016/j.ijpharm.2005.01.018.
- [89] H. Rachmawati, B.M. Haryadi, K. Anggadiredja, V. Suendo, Intraoral film containing insulin-

phospholipid microemulsion: Formulation and in vivo hypoglycemic activity study, *AAPS PharmSciTech.* 16 (2015) 692–703. doi:10.1208/s12249-014-0258-9.

[90] A.K. Agrawal, H. Harde, K. Thanki, S. Jain, Improved stability and antidiabetic potential of insulin containing folic acid functionalized polymer stabilized multilayered liposomes following oral administration, *Biomacromolecules.* 15 (2014) 350–360. doi:10.1021/bm401580k.

[91] R. Sharma, U. Gupta, N.K. Garg, R.K. Tyagi, N.K. Jain, Surface engineered and ligand anchored nanobioconjugate: An effective therapeutic approach for oral insulin delivery in experimental diabetic rats, *Colloids Surfaces B Biointerfaces.* 127 (2015) 172–181. doi:10.1016/j.colsurfb.2015.01.035.

[92] K.B. Chalasani, G.J. Russell-Jones, S.K. Yandrapu, P. V. Diwan, S.K. Jain, A novel vitamin B 12-nanosphere conjugate carrier system for peroral delivery of insulin, *J. Control. Release.* 117 (2007) 421–429. doi:10.1016/j.jconrel.2006.12.003.

[93] F. Cui, K. Shi, L. Zhang, A. Tao, Y. Kawashima, Biodegradable nanoparticles loaded with insulin-phospholipid complex for oral delivery: Preparation, in vitro characterization and in vivo evaluation, *J. Control. Release.* 114 (2006) 242–250. doi:10.1016/j.jconrel.2006.05.013.

[94] Z. Ma, T.M. Lim, L.Y. Lim, Pharmacological activity of peroral chitosan-insulin nanoparticles in diabetic rats, *Int. J. Pharm.* 293 (2005) 271–280. doi:10.1016/j.ijpharm.2004.12.025.

[95] M.A. Radwan, Enhancement of absorption of insulin-loaded polyisobutylcyanoacrylate nanospheres by sodium cholate after oral and subcutaneous administration in diabetic rats., *Drug Dev. Ind. Pharm.* 27 (2001) 981–9. doi:10.1081/DDC-100107680.

[96] S. Sajeesh, K. Bouchemal, V. Marsaud, C. Vauthier, C.P. Sharma, Cyclodextrin complexed insulin encapsulated hydrogel microparticles: An oral delivery system for insulin, *J. Control. Release.* 147 (2010) 377–384. doi:10.1016/j.jconrel.2010.08.007.

[97] W. Wei, G.H. Ma, L.Y. Wang, J. Wu, Z.G. Su, Hollow quaternized chitosan microspheres increase the therapeutic effect of orally administered insulin, *Acta Biomater.* 6 (2010) 205–209. doi:10.1016/j.actbio.2009.06.005.

[98] K. Kesavan, G. Nath, J.K. Pandit, Preparation and in vitro antibacterial evaluation of gatifloxacin mucoadhesive gellan system., *J. Fac. Pharmacy, Tehran Univ. Med. Sci.* 18 (2010) 237–46.

[99] Y. Pan, Y. Li, H. Zhao, J. Zhen, H. Xu, G. Wei, J. Hao, F. Cui, Bioadhesive polysaccharide in protein delivery system: chitosan nanoparticles improve the intestinal absorption of insulin in vivo, *Int. J. Pharm.* 249 (2002) 139–147. doi:10.1016/S0378-5173(02)00486-6.

[100] P.C. Naha, V. Kanchan, P.K. Manna, A.K. Panda, Improved bioavailability of orally delivered insulin using Eudragit-L30D coated PLGA microparticles, *J. Microencapsul.* 25 (2008) 248–256. doi:10.1080/02652040801903843.

[101] L. Sun, X. Zhang, Z. Wu, C. Zheng, C. Li, Oral glucose- and pH-sensitive nanocarriers for simulating insulin release in vivo, *Polym. Chem.* 5 (2014) 1999–2009. doi:10.1039/c3py01416a.

[102] S. Sun, N. Liang, H. Piao, H. Yamamoto, Y. Kawashima, F. Cui, Insulin-S.O (sodium oleate) complex-loaded PLGA nanoparticles: Formulation, characterization and in vivo evaluation, *J. Microencapsul.* 27 (2010) 471–478. doi:10.3109/02652040903515490.

[103] R. Yang, R. Gao, F. Li, H. He, X. Tang, The influence of lipid characteristics on the formation, in vitro release, and in vivo absorption of protein-loaded SLN prepared by the double emulsion process, *Drug Dev. Ind. Pharm.* 37 (2011) 139–48. doi:10.3109/03639045.2010.497151.

[104] L. Zhang, L. Song, C. Zhang, Y. Ren, Improving intestinal insulin absorption efficiency through coadministration of cell-penetrating peptide and hydroxypropyl- β -cyclodextrin, *Carbohydr. Polym.* 87 (2012) 1822–1827. doi:10.1016/j.carbpol.2011.10.002.

[105] P. He, Z. Tang, L. Lin, M. Deng, X. Pang, X. Zhuang, X. Chen, Novel biodegradable and pH-sensitive poly(ester amide) microspheres for oral insulin delivery, *Macromol. Biosci.* 12 (2012) 547–556. doi:10.1002/mabi.201100358.

[106] P. He, H. Liu, Z. Tang, M. Deng, Y. Yang, X. Pang, X. Chen, Poly(ester amide) blend microspheres for oral insulin delivery, *Int. J. Pharm.* 455 (2013) 259–266. doi:10.1016/j.ijpharm.2013.07.022.

- 767 [107] C.J. Lim, W.C. Shen, Comparison of monomeric and oligomeric transferrin as potential carrier in oral
768 delivery of protein drugs, *J. Control. Release.* 106 (2005) 273–286.
769 doi:10.1016/j.jconrel.2005.05.001.
- 770 [108] Y.H. Lin, F.L. Mi, C.T. Chen, W.C. Chang, S.F. Peng, H.F. Liang, H.W. Sung, Preparation and
771 characterization of nanoparticles shelled with chitosan for oral insulin delivery, *Biomacromolecules.*
772 8 (2007) 146–152. doi:10.1021/bm0607776.
- 773 [109] M.R. Rekha, C.P. Sharma, Synthesis and evaluation of lauryl succinyl chitosan particles towards oral
774 insulin delivery and absorption, *J. Control. Release.* 135 (2009) 144–151.
775 doi:10.1016/j.jconrel.2009.01.011.
- 776 [110] G. Sharma, K. Wilson, C.F. van der Walle, N. Sattar, J.R. Petrie, M.N. V Ravi Kumar, Microemulsions
777 for oral delivery of insulin: design, development and evaluation in streptozotocin induced diabetic
778 rats, *Eur. J. Pharm. Biopharm.* 76 (2010) 159–69. doi:10.1016/j.ejpb.2010.07.002.
- 779 [111] K. Sonaje, E.Y. Chuang, K.J. Lin, T.C. Yen, F.Y. Su, M.T. Tseng, H.W. Sung, Opening of epithelial tight
780 junctions and enhancement of paracellular permeation by chitosan: Microscopic, ultrastructural,
781 and computed-tomographic observations, *Mol. Pharm.* 9 (2012) 1271–1279.
782 doi:10.1021/mp200572t.
- 783 [112] T. Trenktrog, B.W. Müller, F.M. Specht, J. Seifert, Enteric coated insulin pellets: Development, drug
784 release and in vivo evaluation, *Eur. J. Pharm. Sci.* 4 (1996) 323–329. doi:10.1016/0928-
785 0987(95)00162-X.
- 786 [113] C.B. Woitiski, R.J. Neufeld, F. Veiga, R.A. Carvalho, I. V. Figueiredo, Pharmacological effect of orally
787 delivered insulin facilitated by multilayered stable nanoparticles, *Eur. J. Pharm. Sci.* 41 (2010) 556–
788 563. doi:10.1016/j.ejps.2010.08.009.
- 789 [114] C.Q. Xia, W.C. Shen, Tyrphostin-8 enhances transferrin receptor-mediated transcytosis in Caco-2
790 cells and increases hypoglycemic effect of orally administered insulin-transferrin conjugate in
791 diabetic rats, *Pharm. Res.* 18 (2001) 191–195. doi:10.1023/A:1011032502097.
- 792 [115] Z. Al-Kurdi, B.Z. Chowdhry, S.A. Leharne, N.A. Qinna, M.M.H. Al-Omari, A.A. Badwan, Influence of
793 glutathione on the bioactivity of subcutaneously or orally administered insulin to rats, *Protein Pept.*
794 *Lett.* 22 (2015) 489–496. doi:0929-8665/15.
- 795 [116] N.A. Qinna, Q.G. Karwi, N. Al-Jbour, M.A. Al-Remawi, T.M. Alhussainy, K.A. Al-So'ud, M.M.H. Al
796 Omari, A.A. Badwan, Influence of molecular weight and degree of deacetylation of low molecular
797 weight chitosan on the bioactivity of oral insulin preparations, *Mar. Drugs.* 13 (2015) 1710–1725.
798 doi:10.3390/md13041710.
- 799 [117] H. Guo, H. Li, J. Gao, G. Zhao, L. Ling, B. Wang, Q. Gui, Y. Gu, C. Li, Phenylboronic acid-based
800 amphiphilic glycopolymeric nanocarriers for in vivo insulin delivery, *Polym. Chem.* 7 (2016) 3189–
801 3199. doi:10.1039/C6PY00131A.
- 802 [118] J. Wang, M. Xu, X. Cheng, M. Kong, Y. Liu, C. Feng, X. Chen, Positive/negative surface charge of
803 chitosan based nanogels and its potential influence on oral insulin delivery, *Carbohydr. Polym.* 136
804 (2016) 867–874. doi:10.1016/j.carbpol.2015.09.103.
- 805 [119] M. Jelvehgari, P.Z. Milani, M.R. Siahi-Shabad, F. Monajjemzadeh, A. Nokhodchi, Z. Azari, H.
806 Valizadeh, In vitro and in vivo evaluation of insulin microspheres containing proteaseinhibitor,
807 *Arzneimittelforschung.* 61 (2011) 14–22.
- 808 [120] R.C. Mundargi, V. Rangaswamy, T.M. Aminabhavi, Poly(N-vinylcaprolactam-co-methacrylic acid)
809 hydrogel microparticles for oral insulin delivery, *J. Microencapsul.* 28 (2011) 384–394.
810 doi:10.3109/02652048.2011.576782.
- 811 [121] E. Lee, J. Lee, S. Jon, A novel approach to oral delivery of insulin by conjugating with low molecular
812 weight chitosan, *Bioconjug. Chem.* 21 (2010) 1720–1723. doi:10.1021/bc100093v.
- 813 [122] B.Y. Kim, J.H. Jeong, K. Park, J.D. Kim, Bioadhesive interaction and hypoglycemic effect of insulin-
814 loaded lectin-microparticle conjugates in oral insulin delivery system, *J. Control. Release.* 102 (2005)
815 525–538. doi:10.1016/j.jconrel.2004.10.032.
- 816 [123] M. Liu, J. Zhang, X. Zhu, W. Shan, L. Li, J. Zhong, Z. Zhang, Y. Huang, Efficient mucus permeation and

817 tight junction opening by dissociable “mucus-inert” agent coated trimethyl chitosan nanoparticles
818 for oral insulin delivery, *J. Control. Release*. 222 (2016) 67–77. doi:10.1016/j.jconrel.2015.12.008.

819 [124] G. Sharma, C.F. Van Der Walle, M.N. V Ravi Kumar, Antacid co-encapsulated polyester nanoparticles
820 for peroral delivery of insulin: Development, pharmacokinetics, biodistribution and
821 pharmacodynamics, *Int. J. Pharm.* 440 (2013) 99–110. doi:10.1016/j.ijpharm.2011.12.038.

822 [125] U. Ubaidulla, Y. Sultana, F.J. Ahmed, R.K. Khar, A.K. Panda, Chitosan phthalate microspheres for oral
823 delivery of insulin: Preparation, characterization, and in vitro evaluation, *Drug Deliv.* 14 (2007) 19–
824 23. doi:10.1080/10717540600559478.

825 [126] H.J. Cho, J. Oh, M.K. Choo, J.I. Ha, Y. Park, H.J. Maeng, Chondroitin sulfate-capped gold nanoparticles
826 for the oral delivery of insulin, *Int. J. Biol. Macromol.* 63 (2014) 15–20.
827 doi:10.1016/j.ijbiomac.2013.10.026.

828 [127] D.R. Bhumkar, H.M. Joshi, M. Sastry, V.B. Pokharkar, Chitosan reduced gold nanoparticles as novel
829 carriers for transmucosal delivery of insulin, *Pharm. Res.* 24 (2007) 1415–1426. doi:10.1007/s11095-
830 007-9257-9.

831 [128] M. Cui, W. Wu, L. Hovgaard, Y. Lu, D. Chen, J. Qi, Liposomes containing cholesterol analogues of
832 botanical origin as drug delivery systems to enhance the oral absorption of insulin, *Int. J. Pharm.* 489
833 (2015) 277–284. doi:10.1016/j.ijpharm.2015.05.006.

834 [129] D. Sakloetsakun, S. Dünnhaupt, J. Barthelmes, G. Perera, A. Bernkop-Schnürch, Combining two
835 technologies: Multifunctional polymers and self-nanoemulsifying drug delivery system (SNEDDS) for
836 oral insulin administration, *Int. J. Biol. Macromol.* 61 (2013) 363–372.
837 doi:10.1016/j.ijbiomac.2013.08.002.

838 [130] A. Viehof, L. Javot, A. Béduneau, Y. Pellequer, A. Lamprecht, Oral insulin delivery in rats by
839 nanoparticles prepared with non-toxic solvents, *Int. J. Pharm.* 443 (2013) 169–174.
840 doi:10.1016/j.ijpharm.2013.01.017.

841 [131] T.A. Sonia, M.R. Rekha, C.P. Sharma, Bioadhesive hydrophobic chitosan microparticles for oral
842 delivery of insulin: In vitro characterization and in vivo uptake studies, *J. Appl. Polym. Sci.* 119 (2011)
843 2902–2910. doi:10.1002/app.32979.

844 [132] M. Alibolandi, F. Alabdollah, F. Sadeghi, M. Mohammadi, K. Abnous, M. Ramezani, F. Hadizadeh,
845 Dextran-b-poly(lactide-co-glycolide) polymersome for oral delivery of insulin: In vitro and in vivo
846 evaluation, *J. Control. Release*. 227 (2016) 58–70. doi:10.1016/j.jconrel.2016.02.031.

847 [133] N. Zhang, Q. Ping, G. Huang, W. Xu, Y. Cheng, X. Han, Lectin-modified solid lipid nanoparticles as
848 carriers for oral administration of insulin, *Int. J. Pharm.* 327 (2006) 153–159.
849 doi:10.1016/j.ijpharm.2006.07.026.

850 [134] E. Ma, H. Ma, Z. Liu, C. Zheng, M. Duan, In vitro and in vivo evaluation of a novel oral insulin
851 formulation, *Acta Pharmacol. Sin.* 27 (2006) 1382–1388. doi:10.1111/j.1745-7245.2006.00424.x.

852 [135] L.K. Tomar, C. Tyagi, S.S. Lahiri, H. Singh, Poly(PEGDMA-MAA) copolymeric micro and nanoparticles
853 for oral insulin delivery, *Polym. Adv. Technol.* 22 (2011) 1760–1767. doi:10.1002/pat.1669.

854 [136] Z. Li, J. Chen, W. Sun, Y. Xu, Investigation of archaeosomes as carriers for oral delivery of peptides,
855 *Biochem. Biophys. Res. Commun.* 394 (2010) 412–417. doi:10.1016/j.bbrc.2010.03.041.

856 [137] H. Sun, D. Liu, Y. Li, X. Tang, Y. Cong, Preparation and in vitro/ in vivo characterization of enteric-
857 coated nanoparticles loaded with the antihypertensive peptide VLPVPR, *Int. J. Nanomedicine*. 9
858 (2014) 1709–1716. doi:10.2147/IJN.S56092.

859 [138] S. Dünnhaupt, J. Barthelmes, J. Iqbal, G. Perera, C.C. Thurner, H. Friedl, A. Bernkop-Schnürch, In vivo
860 evaluation of an oral drug delivery system for peptides based on S-protected thiolated chitosan, *J.*
861 *Control. Release*. 160 (2012) 477–485. doi:10.1016/j.jconrel.2012.04.020.

862 [139] H.L. Luessen, B.J. de Leeuw, M.W. Langemeijer, A.B. de Boer, J.C. Verhoef, H.E. Junginger,
863 Mucoadhesive polymers in peroral peptide drug delivery. VI. Carbomer and chitosan improve the
864 intestinal absorption of the peptide drug buserelin in vivo, *Pharm. Res.* 13 (1996) 1668–1672.
865 doi:10.1023/A:1016488623022.

866 [140] M. Wang, Y. Zhang, J. Feng, T. Gu, Q. Dong, X. Yang, Y. Sun, Y. Wu, Y. Chen, W. Kong, Preparation,

characterization, and in vitro and in vivo investigation of chitosan-coated poly (d,l-lactide-co-glycolide) nanoparticles for intestinal delivery of exendin-4, *Int. J. Nanomedicine*. 8 (2013) 1141–1154. doi:10.2147/IJN.S41457.

[141] C. Chen, X. Zhu, Y. Dou, J. Xu, J. Zhang, T. Fan, J. Du, K. Liu, Y. Deng, L. Zhao, Y. Huang, Exendin-4 loaded nanoparticles with a lipid shell and aqueous core containing micelles for enhanced intestinal absorption, *J. Biomed. Nanotechnol.* 11 (2015) 865–876. doi:10.1166/jbn.2015.1971.

[142] Y.S. Youn, S.Y. Chae, S. Lee, M.J. Kwon, H.J. Shin, K.C. Lee, Improved peroral delivery of glucagon-like peptide-1 by site-specific biotin modification: design, preparation, and biological evaluation, *Eur. J. Pharm. Biopharm.* 68 (2008) 667–75. doi:10.1016/j.ejpb.2007.07.009.

[143] X. Li, C. Wang, R. Liang, F. Sun, Y. Shi, A. Wang, W. Liu, K. Sun, Y. Li, The glucose-lowering potential of exenatide delivered orally via goblet cell- targeting nanoparticles, *Pharm. Res.* 32 (2015) 1017–1027. doi:10.1007/s11095-014-1513-1.

[144] S.Y. Chae, C. Jin, H.J. Shin, Y.S. Youn, S. Lee, K.C. Lee, Preparation, characterization, and application of biotinylated and biotin-PEGylated glucagon-like peptide-1 analogues for enhanced oral delivery, *Bioconjugate Chem.* 19 (2008) 334–341. doi:10.1021/bc700292v.

[145] J.W. Joseph, J. Kalitsky, S. St-Pierre, P.L. Brubaker, Oral delivery of glucagon-like peptide-1 in a modified polymer preparation normalizes basal glycaemia in diabetic db/db mice, *Diabetologia*. 43 (2000) 1319–28. doi:10.1007/s001250051529.

[146] N. Shrestha, F. Araújo, M.-A. Shahbazi, E. Mäkilä, M.J. Gomes, M. Airavaara, E.I. Kauppinen, J. Raula, J. Salonen, J. Hirvonen, B. Sarmiento, H.A. Santos, Oral hypoglycaemic effect of GLP-1 and DPP4 inhibitor based nanocomposites in a diabetic animal model, *J. Control. Release*. 232 (2016) 113–119. doi:10.1016/j.jconrel.2016.04.024.

[147] F. Araújo, N. Shrestha, M.A. Shahbazi, D. Liu, B. Herranz-Blanco, E.M. Mäkilä, J.J. Salonen, J.T. Hirvonen, P.L. Granja, B. Sarmiento, H.A. Santos, Microfluidic assembly of a multifunctional tailorable composite system designed for site specific combined oral delivery of peptide drugs, *ACS Nano*. 9 (2015) 8291–8302. doi:10.1021/acsnano.5b02762.

[148] F.-Y. Su, E.-Y. Chuang, P.-Y. Lin, Y.-C. Chou, C.-T. Chen, F.-L. Mi, S.-P. Wey, T.-C. Yen, K.-J. Lin, H.-W. Sung, Treatment of chemotherapy-induced neutropenia in a rat model by using multiple daily doses of oral administration of G-CSF-containing nanoparticles, *Biomaterials*. 35 (2014) 3641–9. doi:10.1016/j.biomaterials.2014.01.020.

[149] Z. Khatun, Nurunnabi, K.J. Cho, Y. Byun, Y.H. Bae, Y. Lee, Oral absorption mechanism and anti-angiogenesis effect of taurocholic acid-linked heparin-docetaxel conjugates, *J. Control. Release*. 177 (2014) 64–73. doi:10.1016/j.jconrel.2013.12.034.

[150] Y. Zheng, Y. Qiu, M.F. Lu, D. Hoffman, T.L. Reiland, Permeability and absorption of leuprolide from various intestinal regions in rabbits and rats, *Int. J. Pharm.* 185 (1999) 83–92. doi:10.1016/S0378-5173(99)00146-5.

[151] J. Iqbal, C. Vigl, G. Moser, M. Gasteiger, G. Perera, A. Bernkop-Schnürch, Development and in vivo evaluation of a new oral nanoparticulate dosage form for leuprolide based on polyacrylic acid, *Drug Deliv.* 18 (2011) 432–40. doi:10.3109/10717544.2011.577108.

[152] P. Uhl, F. Helm, G. Hofhaus, S. Brings, C. Kaufman, K. Leotta, S. Urban, U. Haberkorn, W. Mier, G. Fricker, A liposomal formulation for the oral application of the investigational hepatitis B drug Myrcludex B, *Eur. J. Pharm. Biopharm.* 103 (2016) 159–166. doi:10.1016/j.ejpb.2016.03.031.

[153] S.A. Moreno-Mendieta, D. Guillén, C. Espitia, R. Hernández-Pando, S. Sanchez, R. Rodríguez-Sanoja, A novel antigen-carrier system: the Mycobacterium tuberculosis Acr protein carried by raw starch microparticles, *Int. J. Pharm.* 474 (2014) 241–8. doi:10.1016/j.ijpharm.2014.07.041.

[154] T.A.S. Aguirre, M. Rosa, I.S. Coulter, D.J. Brayden, In vitro and in vivo preclinical evaluation of a minisphere emulsion-based formulation (SmPill®) of salmon calcitonin, *Eur. J. Pharm. Sci.* 79 (2015) 102–111. doi:10.1016/j.ejps.2015.09.001.

[155] P.J. Sinko, Y.H. Lee, V. Makhey, G.D. Leesman, J.P. Sutyak, H. Yu, B. Perry, C.L. Smith, P. Hu, W.E. J, L.M. Falzone, L.T. McWhorter, J.P. Gilligan, W. Stern, Biopharmaceutical approaches for developing

and assessing oral peptide delivery strategies and systems: in vitro permeability and in vivo oral absorption of salmon calcitonin (sCT), *Pharm. Res.* 16 (1999) 527–533. doi:10.1023/A:1018819012405.

[156] V. Gupta, B.H. Hwang, N. Doshi, S. Mitragotri, A permeation enhancer for increasing transport of therapeutic macromolecules across the intestine, *J. Control. Release.* 172 (2013) 541–549. doi:10.1016/j.jconrel.2013.05.002.

[157] V. Gupta, B.H. Hwang, J. Lee, A.C. Anselmo, N. Doshi, S. Mitragotri, Mucoadhesive intestinal devices for oral delivery of salmon calcitonin, *J. Control. Release.* 172 (2013) 753–762. doi:10.1016/j.jconrel.2013.09.004.

[158] W.-P. Cheng, C. Thompson, S.M. Ryan, T. Aguirre, L. Tetley, D.J. Brayden, In vitro and in vivo characterisation of a novel peptide delivery system: amphiphilic polyelectrolyte-salmon calcitonin nanocomplexes, *J. Control. Release.* 147 (2010) 289–97. doi:10.1016/j.jconrel.2010.07.128.

[159] M. Cetin, Y.S. Youn, Y. Capan, K.C. Lee, Preparation and characterization of salmon calcitonin-biotin conjugates, *AAPS PharmSciTech.* 9 (2008) 1191–7. doi:10.1208/s12249-008-9165-2.

[160] D. Guggi, C.E. Kast, A. Bernkop-Schnürch, In vivo evaluation of an oral salmon calcitonin-delivery system based on a thiolated chitosan carrier matrix, *Pharm. Res.* 20 (2003) 1989–1994. doi:0724-8741/03/1200-1989/0.

[161] H.E. Lee, M.J. Lee, C.R. Park, A.Y. Kim, K.H. Chun, H.J. Hwang, D.H. Oh, S.O. Jeon, J.S. Kang, T.S. Jung, G.J. Choi, S. Lee, Preparation and characterization of salmon calcitonin–sodium triphosphate ionic complex for oral delivery, *J. Control. Release.* 143 (2010) 251–257. doi:10.1016/j.jconrel.2009.12.011.

[162] A. Huang, A. Makhlof, Q. Ping, Y. Tozuka, H. Takeuchi, N-trimethyl chitosan-modified liposomes as carriers for oral delivery of salmon calcitonin, *Drug Deliv.* 18 (2011) 562–569. doi:10.3109/10717544.2011.596585.

[163] A. Makhlof, M. Werle, Y. Tozuka, H. Takeuchi, A mucoadhesive nanoparticulate system for the simultaneous delivery of macromolecules and permeation enhancers to the intestinal mucosa, *J. Control. Release.* 149 (2011) 81–88. doi:10.1016/j.jconrel.2010.02.001.

[164] A. Makhlof, S. Fujimoto, Y. Tozuka, H. Takeuchi, In vitro and in vivo evaluation of WGA-carbopol modified liposomes as carriers for oral peptide delivery, *Eur. J. Pharm. Biopharm.* 77 (2011) 216–24. doi:10.1016/j.ejpb.2010.12.008.

[165] M. Cetin, M.S. Aktas, I. Vural, M. Ozturk, Salmon calcitonin-loaded Eudragit® and Eudragit®-PLGA nanoparticles: In vitro and in vivo evaluation, *J. Microencapsul.* 29 (2012) 156–66. doi:10.3109/02652048.2011.635426.

[166] M. Werle, H. Takeuchi, Chitosan-aprotinin coated liposomes for oral peptide delivery: Development, characterisation and in vivo evaluation, *Int. J. Pharm.* 370 (2009) 26–32. doi:10.1016/j.ijpharm.2008.11.013.

[167] N. Thirawong, J. Thongborisute, H. Takeuchi, P. Srimornsak, Improved intestinal absorption of calcitonin by mucoadhesive delivery of novel pectin-liposome nanocomplexes, *J. Control. Release.* 125 (2008) 236–45. doi:10.1016/j.jconrel.2007.10.023.

[168] C. Prego, D. Torres, E. Fernandez-Megia, R. Novoa-Carballal, E. Quiñoá, M.J. Alonso, Chitosan-PEG nanocapsules as new carriers for oral peptide delivery. Effect of chitosan pegylation degree, *J. Control. Release.* 111 (2006) 299–308. doi:10.1016/j.jconrel.2005.12.015.

[169] M. Garcia-Fuentes, C. Prego, D. Torres, M.J. Alonso, A comparative study of the potential of solid triglyceride nanostructures coated with chitosan or poly(ethylene glycol) as carriers for oral calcitonin delivery, *Eur. J. Pharm. Sci.* 25 (2005) 133–43. doi:10.1016/j.ejps.2005.02.008.

[170] K. Gradauer, J. Barthelmes, C. Vonach, G. Almer, H. Mangge, B. Teubl, E. Roblegg, S. Dünnhaupt, E. Fröhlich, A. Bernkop-Schnürch, R. Prassl, Liposomes coated with thiolated chitosan enhance oral peptide delivery to rats, *J. Control. Release.* 172 (2013) 872–878. doi:10.1016/j.jconrel.2013.10.011.

[171] J. Manosroi, W. Lohcharoenkal, F. Götz, R.G. Werner, W. Manosroi, A. Manosroi, Novel application of polioviral capsid: development of a potent and prolonged oral calcitonin using polioviral binding

- ligand and Tat peptide, *Drug Dev. Ind. Pharm.* 40 (2014) 1092–100. doi:10.3109/03639045.2013.809533.
- [172] H.S. Yoo, T. Park, Biodegradable nanoparticles containing protein-fatty acid complexes for oral delivery of salmon calcitonin, *J. Pharm. Sci.* 93 (2004) 488–495. doi:10.1002/jps.10573.
- [173] I. Lozoya-Agullo, M. Zur, O. Wolk, A. Beig, I. González-Álvarez, M. González-Álvarez, M. Merino-Sanjuán, M. Bermejo, A. Dahan, In-situ intestinal rat perfusions for human Fabs prediction and BCS permeability class determination: Investigation of the single-pass vs. the Doluisio experimental approaches, *Int. J. Pharm.* 480 (2015) 1–7. doi:10.1016/j.ijpharm.2015.01.014.
- [174] I. Lozoya-Agullo, M. Zur, A. Beig, N. Fine, Y. Cohen, M. González-Álvarez, M. Merino-Sanjuán, I. González-Álvarez, M. Bermejo, A. Dahan, Segmental-dependent permeability throughout the small intestine following oral drug administration: Single-pass vs. Doluisio approach to in-situ rat perfusion, *Int. J. Pharm.* 515 (2016) 201–208. doi:10.1016/j.ijpharm.2016.09.061.
- [175] U. Fagerholm, M. Johansson, H. Lennernäs, Comparison between permeability coefficients in rat and human jejunum, *Pharm. Res.* 13 (1996) 1336–1342. doi:10.1023/A:1016065715308.
- [176] X. Cao, S.T. Gibbs, L. Fang, H.A. Miller, C.P. Landowski, H.C. Shin, H. Lennernäs, Y. Zhong, G.L. Amidon, L.X. Yu, D. Sun, Why is it challenging to predict intestinal drug absorption and oral bioavailability in human using rat model, *Pharm. Res.* 23 (2006) 1675–1686. doi:10.1007/s11095-006-9041-2.
- [177] M.A. Lopes, B.A. Abraham, L.M. Cabral, C.R. Rodrigues, R.M.F. Seíça, F.J. de Baptista Veiga, A.J. Ribeiro, Intestinal absorption of insulin nanoparticles: Contribution of M cells, *Nanomedicine Nanotechnology, Biol. Med.* 10 (2014) 1139–1151. doi:10.1016/j.nano.2014.02.014.
- [178] H.J. Van Kruiningen, A.B. West, B.J. Freda, K.A. Holmes, Distribution of Peyer's patches in the distal ileum, *Inflamm. Bowel Dis.* 8 (2002) 180–185. doi:10.1097/00054725-200205000-00004.
- [179] H. Lennernäs, Regional intestinal drug permeation: Biopharmaceutics and drug development, *Eur. J. Pharm. Sci.* 57 (2014) 333–341. doi:10.1016/j.ejps.2013.08.025.
- [180] H. Lennernäs, S. Nylander, A.-L. Ungell, Jejunal permeability: A comparison between Ussing chambers and in humans, *Pharm. Res.* 14 (1997) 667–671.
- [181] P. Zhang, Y. Xu, X. Zhu, Y. Huang, Goblet cell targeting nanoparticle containing drug-loaded micelle cores for oral delivery of insulin, *Int. J. Pharm.* 496 (2015) 993–1005. doi:10.1016/j.ijpharm.2015.10.078.
- [182] W.H. Barr, S. Riegelman, Intestinal drug absorption and metabolism I: Comparison of methods and models to study physiological factors of in vitro and in vivo intestinal absorption, *J. Pharm. Sci.* 59 (1970) 154–163. doi:10.1002/jps.2600590204.
- [183] A. Jain, S.K. Jain, l-Valine appended PLGA nanoparticles for oral insulin delivery, *Acta Diabetol.* (2015) 663–676. doi:10.1007/s00592-015-0714-3.
- [184] H. van de Waterbeemd, E. Gifford, ADMET in silico modelling: towards prediction paradise?, *Nat. Rev. Drug Discov.* 2 (2003) 192–204. doi:10.1038/nrd1032.
- [185] S.H. Welling, L.K.H. Clemmensen, S.T. Buckley, L. Hovgaard, P.B. Brockhoff, H.H.F. Refsgaard, In silico modelling of permeation enhancement potency in Caco-2 monolayers based on molecular descriptors and random forest, *Eur. J. Pharm. Biopharm.* 94 (2015) 152–159. doi:10.1016/j.ejpb.2015.05.012.
- [186] E. Sjögren, H. Thörn, C. Tannergren, In silico modeling of gastrointestinal drug absorption: predictive performance of three physiologically based absorption models, *Mol. Pharm.* (2016). doi:10.1021/acs.molpharmaceut.5b00861.
- [187] W. Jiang, S. Kim, X. Zhang, R.A. Lionberger, B.M. Davit, D.P. Conner, L.X. Yu, The role of predictive biopharmaceutical modeling and simulation in drug development and regulatory evaluation, *Int. J. Pharm.* 418 (2011) 151–160. doi:10.1016/j.ijpharm.2011.07.024.
- [188] A. Dokoumetzidis, P. Macheras, IIVC of controlled release formulations: Physiological–dynamical reasons for their failure, *J. Control. Release.* 129 (2008) 76–78. doi:10.1016/j.jconrel.2008.04.005.
- [189] E.L. McConnell, A.W. Basit, S. Murdan, Measurements of rat and mouse gastrointestinal pH, fluid

and lymphoid tissue, and implications for in-vivo experiments, *J. Pharm. Pharmacol.* 60 (2008) 63–70. doi:10.1211/jpp.60.1.0008.

[190] A.J.F. King, The use of animal models in diabetes research, *Br. J. Pharmacol.* 166 (2012) 877–894. doi:10.1111/j.1476-5381.2012.01911.x.

[191] S.J. Morgan, C.S. Elangbam, S. Berens, E. Janovitz, A. Vitsky, T. Zabka, L. Conour, Use of animal models of human disease for nonclinical safety assessment of novel pharmaceuticals, *Toxicol. Pathol.* 0 (2012) 1–11. doi:10.1177/0192623312457273.

[192] B.O. Roep, M. Atkinson, M. von Herrath, Satisfaction (not) guaranteed: re-evaluating the use of animal models of type 1 diabetes, *Nat Rev Immunol.* 4 (2004) 989–997. 10.1038/nri1502.

[193] T.S. Fröde, Y.S. Medeiros, Animal models to test drugs with potential antidiabetic activity, *J. Ethnopharmacol.* 115 (2008) 173–183. doi:10.1016/j.jep.2007.10.038.

[194] M. a Valentovic, N. Alejandro, A. Betts Carpenter, P.I. Brown, K. Ramos, Streptozotocin (STZ) diabetes enhances benzo(alpha)pyrene induced renal injury in Sprague Dawley rats, *Toxicol. Lett.* 164 (2006) 214–20. doi:10.1016/j.toxlet.2005.12.009.

[195] Y.-C. Lei, J.-S. Hwang, C.-C. Chan, C.-T. Lee, T.-J. Cheng, Enhanced oxidative stress and endothelial dysfunction in streptozotocin-diabetic rats exposed to fine particles, *Environ. Res.* 99 (2005) 335–43. doi:10.1016/j.envres.2005.03.011.

[196] F. Franconi, G. Seghieri, S. Canu, E. Straface, I. Campesi, W. Malorni, Are the available experimental models of type 2 diabetes appropriate for a gender perspective?, *Pharmacol. Res.* 57 (2008) 6–18. doi:10.1016/j.phrs.2007.11.007.

[197] J.L. Bussiere, P. Martin, M. Horner, J. Couch, M. Flaherty, L. Andrews, J. Beyer, C. Horvath, Alternative strategies for toxicity testing of species-specific biopharmaceuticals, *Int. J. Toxicol.* 28 (2009) 230–53. doi:10.1177/1091581809337262.

[198] D.K. Badyal, H. Lata, A.P. Dadhich, Animal models of hypertension and effect of drugs, *Indian J. Pharmacol.* 35 (2003) 349–362. doi:10.1155/2015/528757.

[199] J.A. Auer, A. Goodship, S. Arnoczky, S. Pearce, J. Price, L. Claes, B. von Rechenberg, M. Hofmann-Amttenbrinck, E. Schneider, R. Müller-Terpitz, F. Thiele, K.-P. Rippe, D.W. Grainger, Refining animal models in fracture research: seeking consensus in optimising both animal welfare and scientific validity for appropriate biomedical use., *BMC Musculoskelet. Disord.* 8 (2007) 72. doi:10.1186/1471-2474-8-72.

[200] L. Pénicaud, P. Ferré, J. Kande, A. Leturque, T. Issad, J. Girard, Effect of anesthesia on glucose production and utilization in rats, *Am. J. Physiol. - Endocrinol. Metab.* 252 (1987) E365–E369. doi:10.1172/JCI111133.

[201] P. V Turner, T. Brabb, C. Pekow, M.A. Vasbinder, Administration of substances to laboratory animals: routes of administration and factors to consider, *J. Am. Assoc. Lab. Anim. Sci.* 50 (2011) 600–613.

[202] A.F. Hoggatt, J. Hoggatt, M. Honerlaw, L.M. Pelus, A spoonful of sugar helps the medicine go down: a novel technique to improve oral gavage in mice, *J. Am. Assoc. Lab. Anim. Sci.* 49 (2010) 329–334.

[203] K. Ōkva, E. Tamoševičiute, A. Čižiute, P. Pokk, O. Rukšenas, T. Nevalainen, Refinements for intragastric gavage in rats, *Scand. J. Lab. Anim. Sci.* 33 (2006) 243–252.

[204] M. Bonnicksen, N. Dragsted, A.K. Hansen, The welfare impact of gavaging laboratory rats, *Anim. Welf.* 14 (2005) 223–227.

[205] S. Saphier, A. Rosner, R. Brandeis, Y. Karton, Gastro intestinal tracking and gastric emptying of solid dosage forms in rats using X-ray imaging, *Int. J. Pharm.* 388 (2010) 190–195. doi:10.1016/j.ijpharm.2010.01.001.

[206] W.P. Norred, A simple method for intragastric administration of powdered materials to rats, *Lab. Anim. Sci.* 33 (1983) 585–586.

[207] P. V Turner, C. Pekow, M.A. Vasbinder, T. Brabb, Administration of substances to laboratory animals: equipment considerations, vehicle selection, and solute preparation, *J. Am. Assoc. Lab. Anim. Sci.* 50 (2011) 614–27.

[208] S. Parasuraman, R. Raveendran, R. Kesavan, Blood sample collection in small laboratory animals, *J.*

1067 Pharmacol. Pharmacother. 1 (2010) 87. doi:10.4103/0976-500X.72350.

1068 [209] S. Harloff-Helleberg, L.A.L. Fliervoet, M. Fanø, M. Schmitt, M. Antopolski, A. Urrti, H.M. Nielsen,

1069 Biophysical characterization and in vivo evaluation of sucrose ester-based gels as carriers for oral

1070 delivery of biopharmaceuticals, Submitted. (2016).

1071 [210] Q. Jin, L. Feng, D.D. Wang, J.J. Wu, J. Hou, Z.R. Dai, S.G. Sun, J.Y. Wang, G.B. Ge, J.N. Cui, L. Yang, A

1072 highly selective near-infrared fluorescent probe for carboxylesterase 2 and its bioimaging

1073 applications in living cells and animals, Biosens. Bioelectron. 83 (2016) 193–199.

1074 doi:10.1016/j.bios.2016.04.075.

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1080
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Captions

Figure 1: Graphic showing the *in vivo* barriers in the intestine following oral administration.

Figure 2: Overview of methods used to evaluate oral bioavailability of insulin (A) and other biopharmaceuticals (B) *in vivo*, *ex vivo* and *in situ* based on reviewed papers listed in Table 1 and 2.

Figure 3: Overview of species used to evaluate oral bioavailability of insulin (A) and other biopharmaceuticals (B) *in vivo*, *in situ* or *ex vivo*. The data are based on reviewed papers, listed in Table 1 and 2.

Figure 4: Effect of anesthesia on blood glucose level in healthy rats after subcutaneous (SC) dosing of insulin. The black arrows indicate momentary inhalation of isoflurane. The curves represent the average of three rats \pm SEM, except for the negative control where n=1. Blood samples were collected via the sublingual tongue vein.

Figure 5: Overview of sampling methods used to evaluate oral bioavailability of insulin (A) and other biopharmaceuticals (B) following *in vivo*, *in situ* or *ex vivo* studies. The graphs are based on the reviewed papers listed in Table 1 and 2.

Figure 6: Overview of the analytical methods used to evaluate oral bioavailability of insulin (A) and other biopharmaceuticals (B) *in vivo*, *in situ* or *ex vivo*. This is based on the reviewed papers listed in Table 1 and 2.

